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(12) **United States Patent**  
**Imran**

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(54) **DEVICE, SYSTEM AND METHODS FOR THE ORAL DELIVERY OF THERAPEUTIC COMPOUNDS**

USPC ..... 604/93.01, 95.01, 95.03, 96.01, 103.01,  
604/103.02, 131–136, 140–146, 153, 156,  
604/157, 173, 890.1, 891.1, 892.1;  
600/117, 118, 160, 128/897–899

(75) Inventor: **Mir Imran**, Los Altos Hills, CA (US)

See application file for complete search history.

(73) Assignee: **Rani Therapeutics, LLC**, San Jose, CA (US)

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(\*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

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EP 2196131 A1 6/2010

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**Related U.S. Application Data**

(63) Continuation-in-part of application No. 12/978,233, filed on Dec. 23, 2010, now Pat. No. 8,721,620, and a continuation-in-part of application No. 12/978,301, filed on Dec. 23, 2010, now Pat. No. 8,562,589.

*Primary Examiner* — Kami A Bosworth

(74) *Attorney, Agent, or Firm* — Wilson Sonsini Goodrich & Rosati

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(57)

**ABSTRACT**

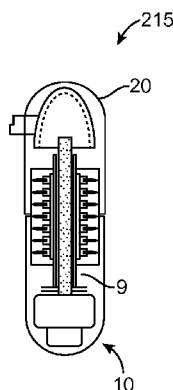
(51) **Int. Cl.**  
**A61M 31/00** (2006.01)  
**A61K 9/00** (2006.01)  
(Continued)

Embodiments of the invention provide swallowable devices, preparations and methods for delivering drugs and other therapeutic agents within the GI tract. Particular embodiments provide a swallowable device such as a capsule for delivering drugs into the intestinal wall or other GI lumen. Embodiments also provide various drug preparations that are configured to be contained within the capsule, advanced from the capsule into the intestinal wall and degrade within the wall to release the drug to produce a therapeutic effect. The preparation can be coupled to a delivery mechanism having one or more balloons or other expandable devices which are expandable responsive to a condition in the small intestine or other GI lumen to advance the preparation out of the capsule into the intestinal wall. Embodiments of the invention are particularly useful for the delivery of drugs which are poorly absorbed, tolerated and/or degraded within the GI tract.

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CPC ..... **A61M 31/002** (2013.01); **A61K 9/0004** (2013.01); **A61K 9/4808** (2013.01);  
(Continued)

(58) **Field of Classification Search**  
CPC ..... A61M 31/002; A61M 37/00; A61M 37/0015; A61M 37/0069; A61M 2037/0023; A61M 2037/003

**16 Claims, 38 Drawing Sheets**



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**A61K 38/21** (2006.01)  
**A61K 38/26** (2006.01)  
**A61K 38/27** (2006.01)  
**A61K 38/28** (2006.01)  
**A61K 38/29** (2006.01)  
**A61M 37/00** (2006.01)
- (52) **U.S. Cl.**  
CPC ..... **A61K 38/21** (2013.01); **A61K 38/26** (2013.01); **A61K 38/27** (2013.01); **A61K 38/28** (2013.01); **A61K 38/29** (2013.01); **A61M 37/0069** (2013.01)
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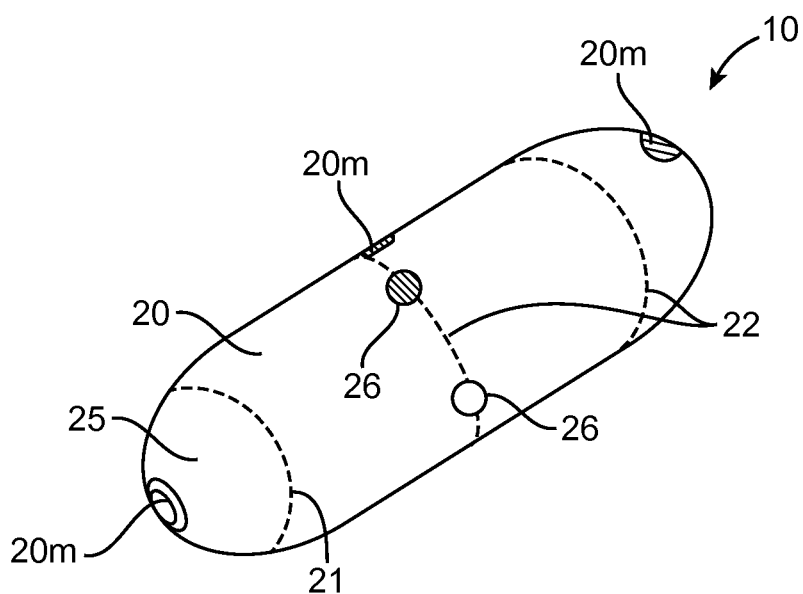


FIG. 1a

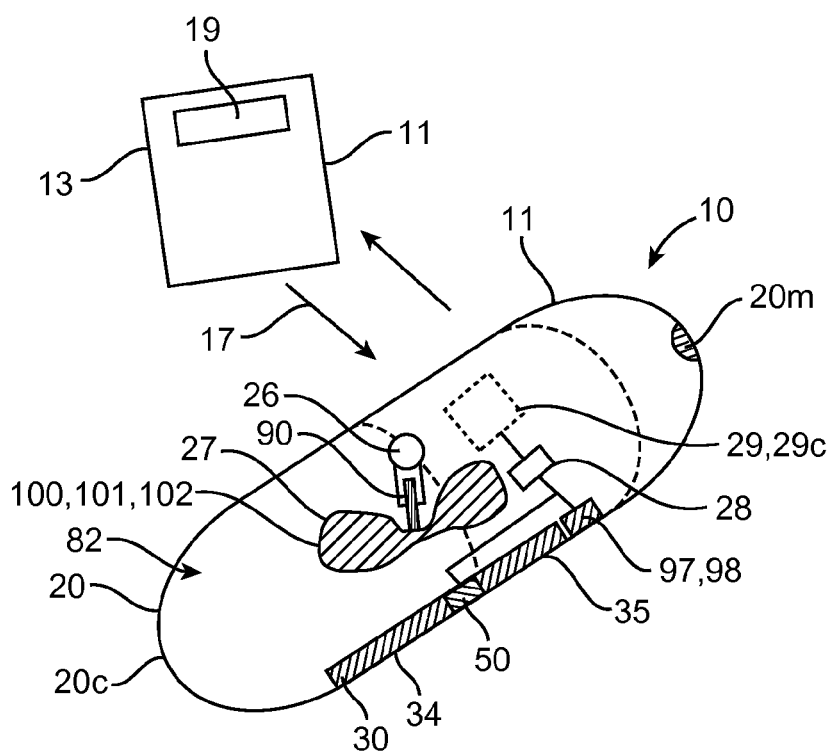


FIG. 1b

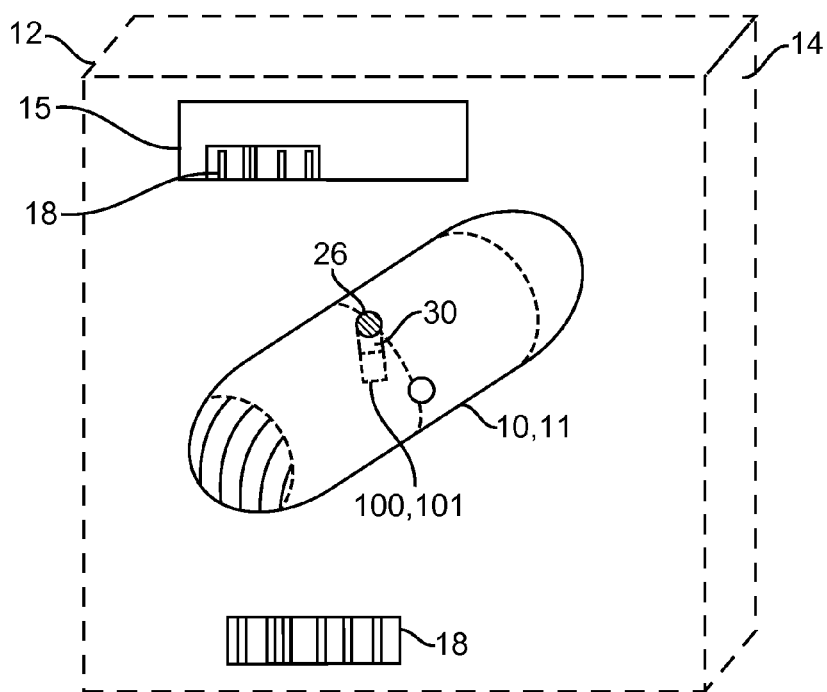


FIG. 1c

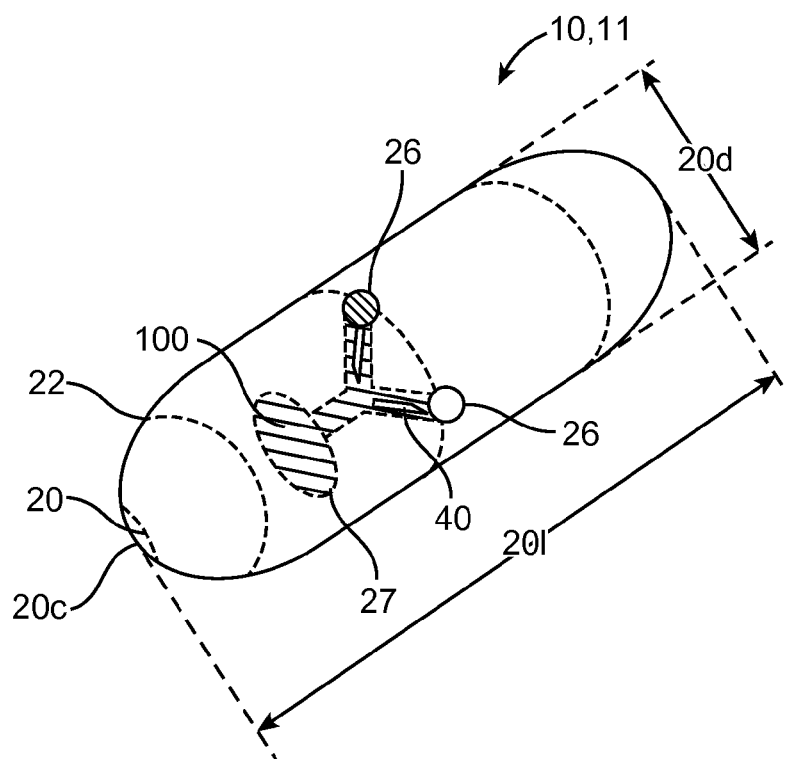


FIG. 1d

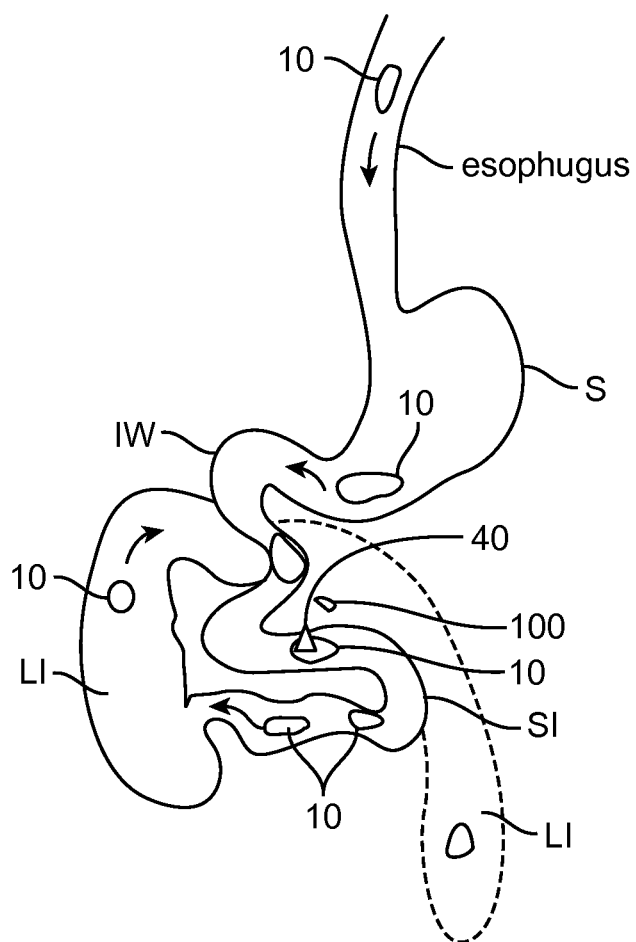


FIG. 1e

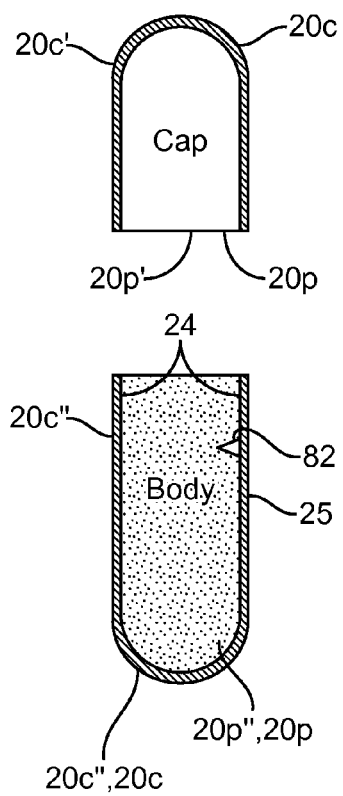


FIG. 2a

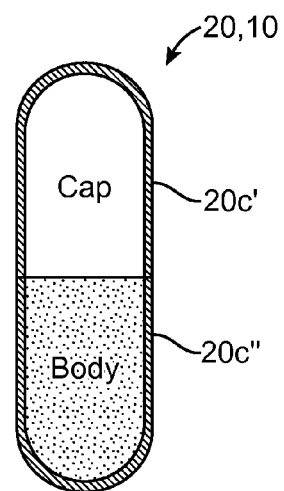
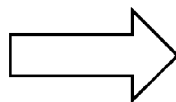


FIG. 2b

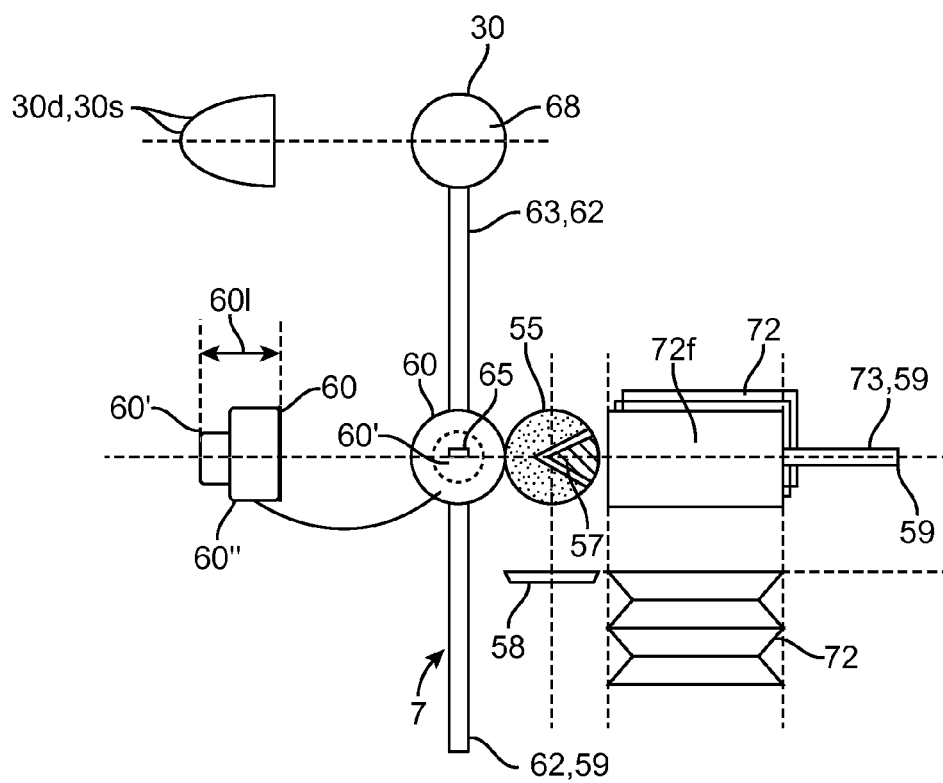


FIG. 3a

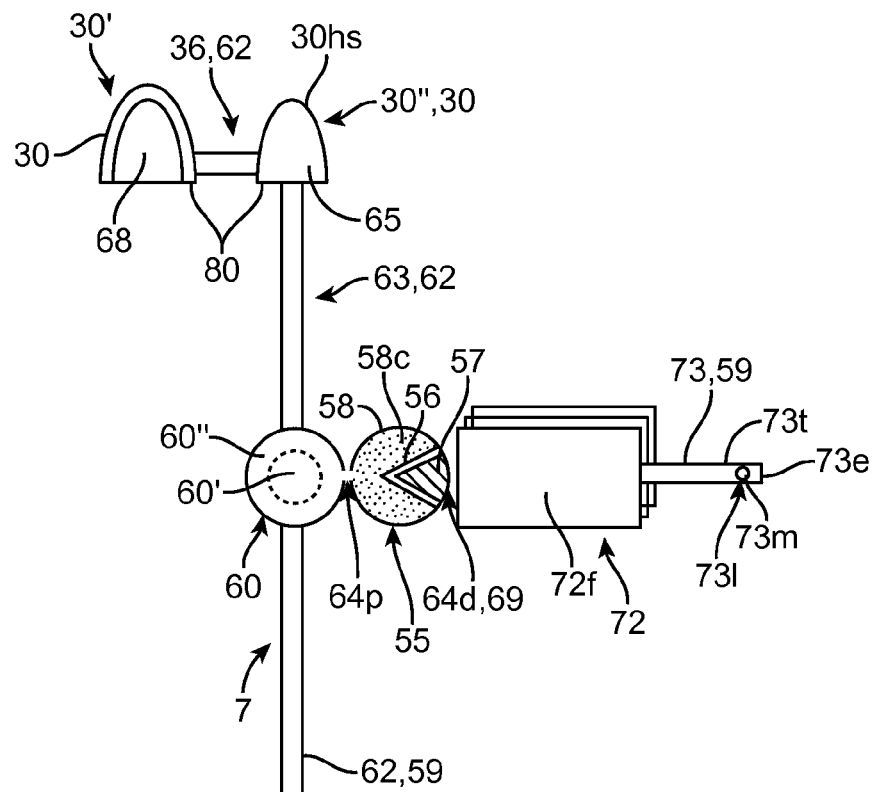


FIG. 3b

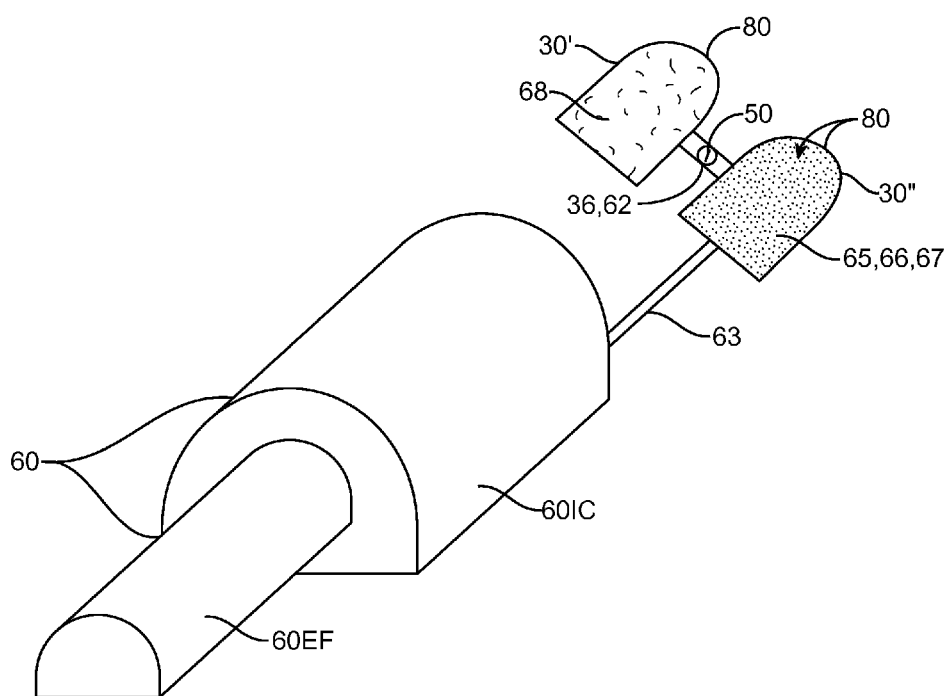


FIG. 3c

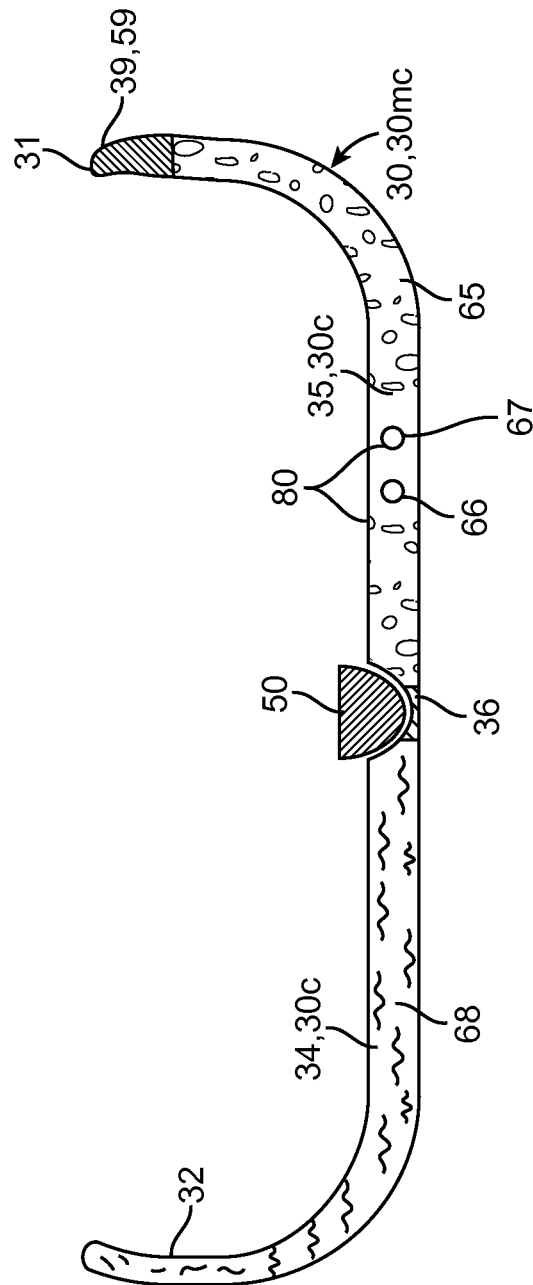


FIG. 4a

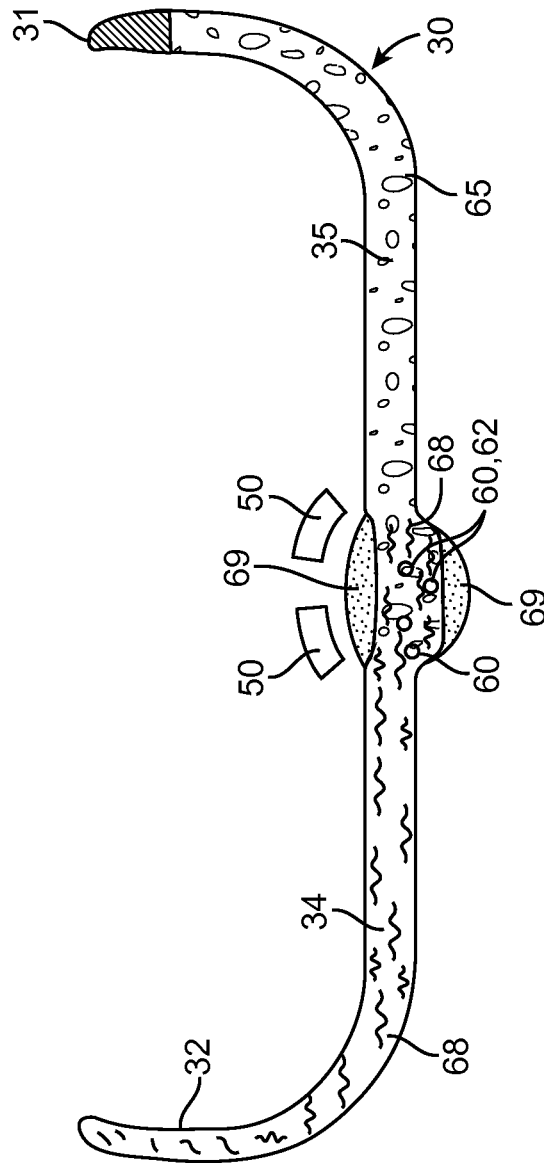


FIG. 4b

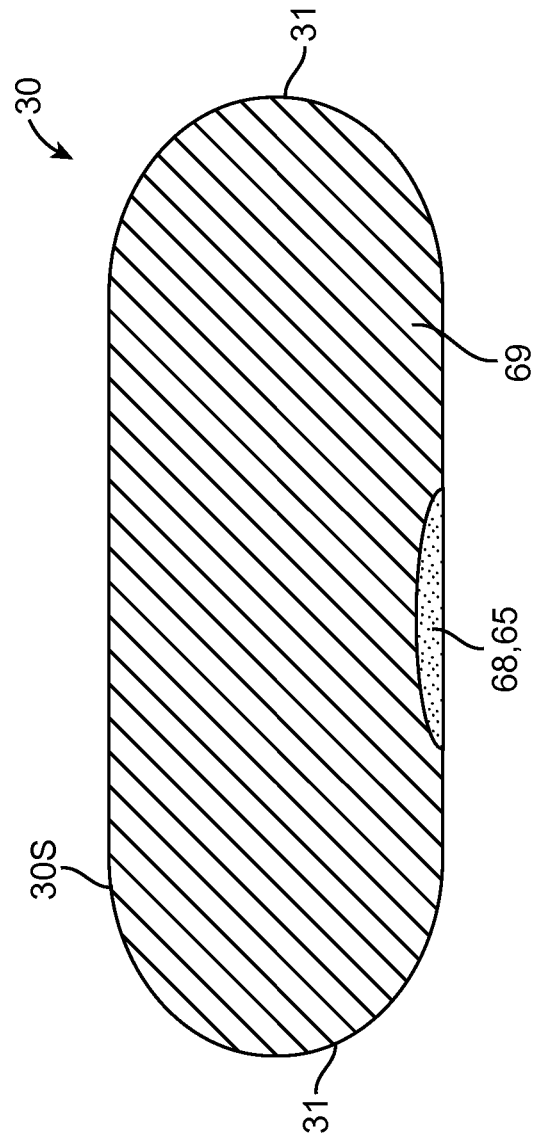


FIG. 4c

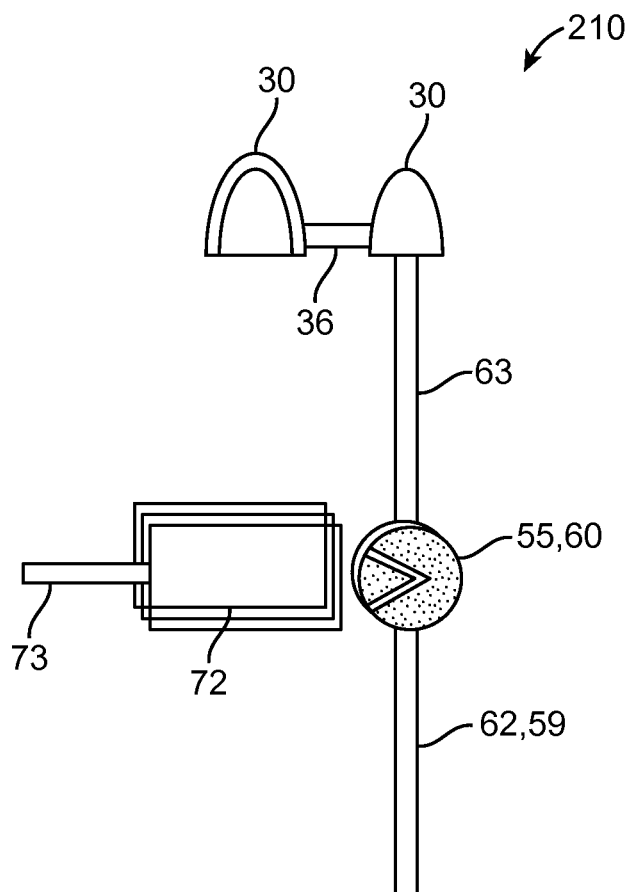


FIG. 5a

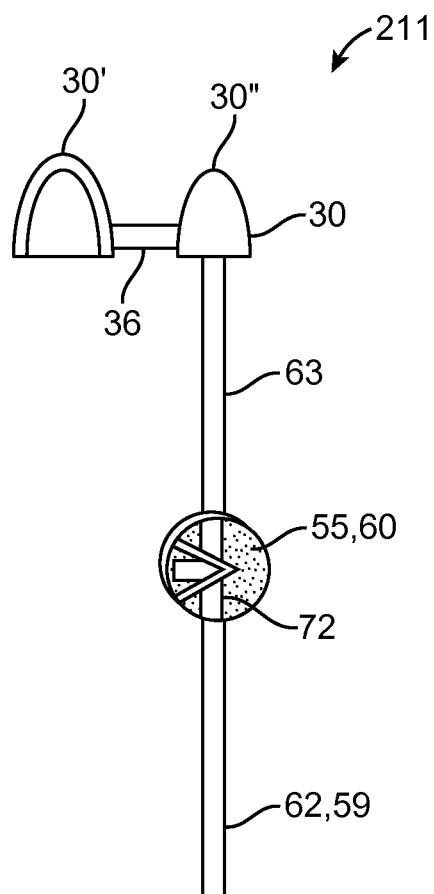


FIG. 5b

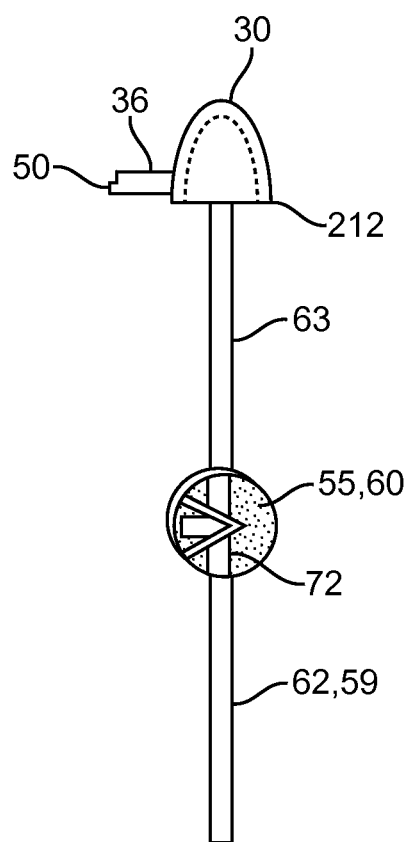


FIG. 5c

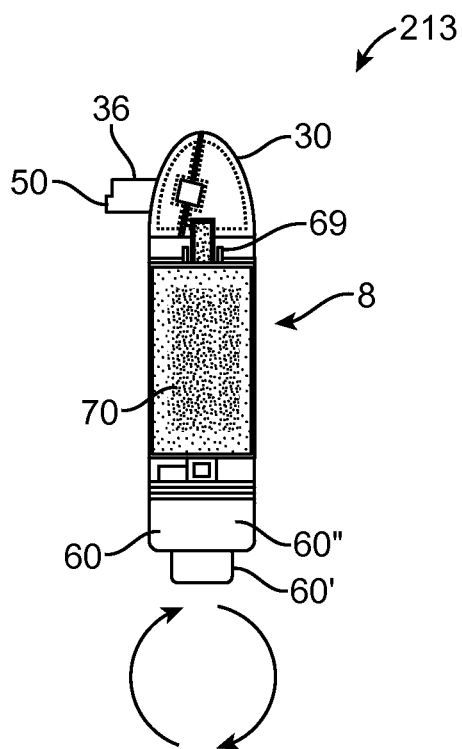


FIG. 5d

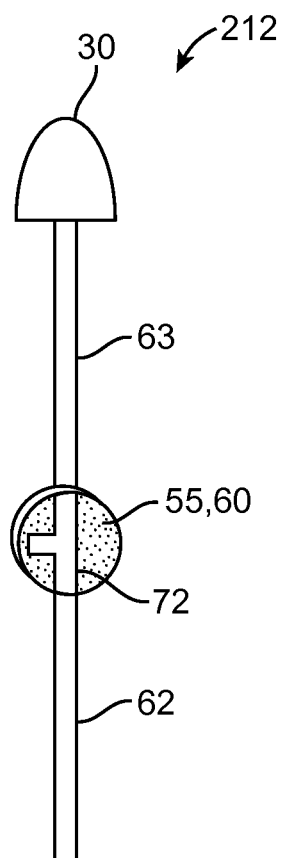


FIG. 5e

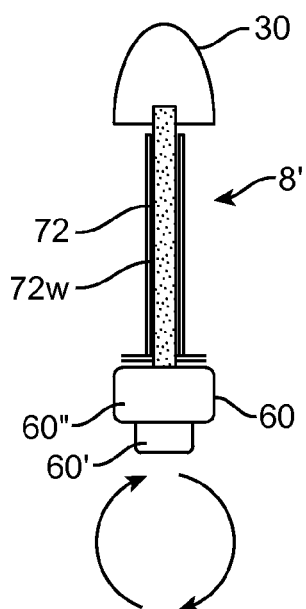


FIG. 5f

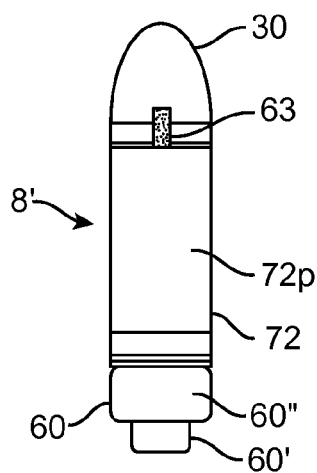


FIG. 5g

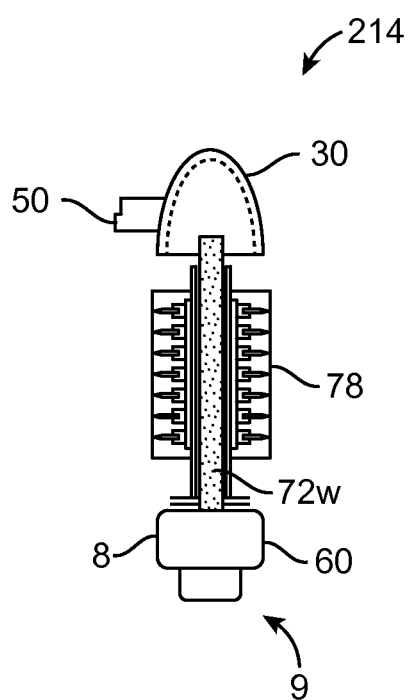


FIG. 6a

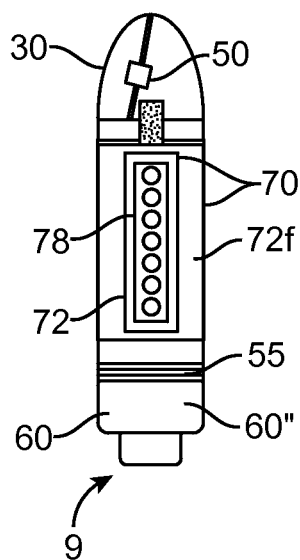


FIG. 6b

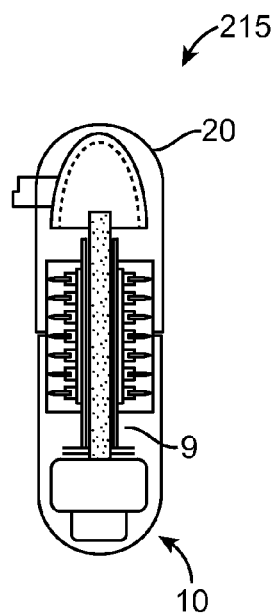


FIG. 7a

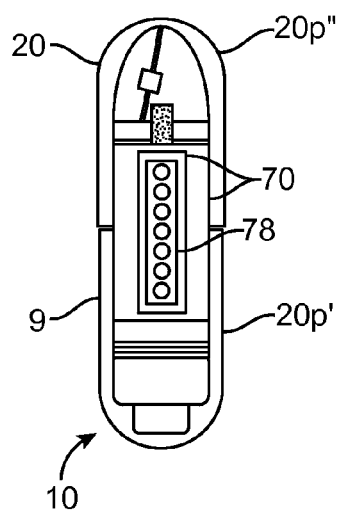


FIG. 7b

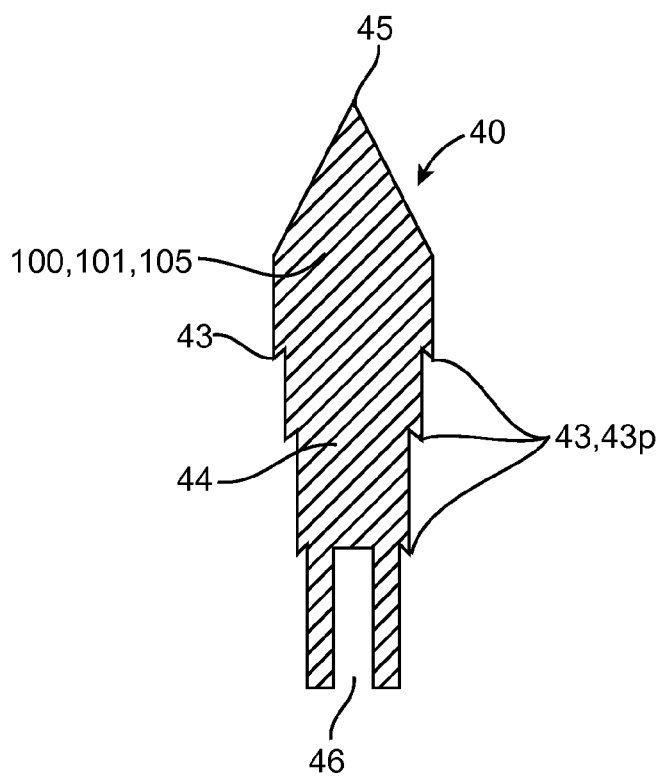


FIG. 8a

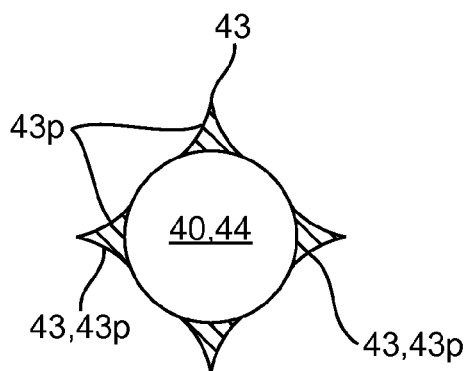


FIG. 8b

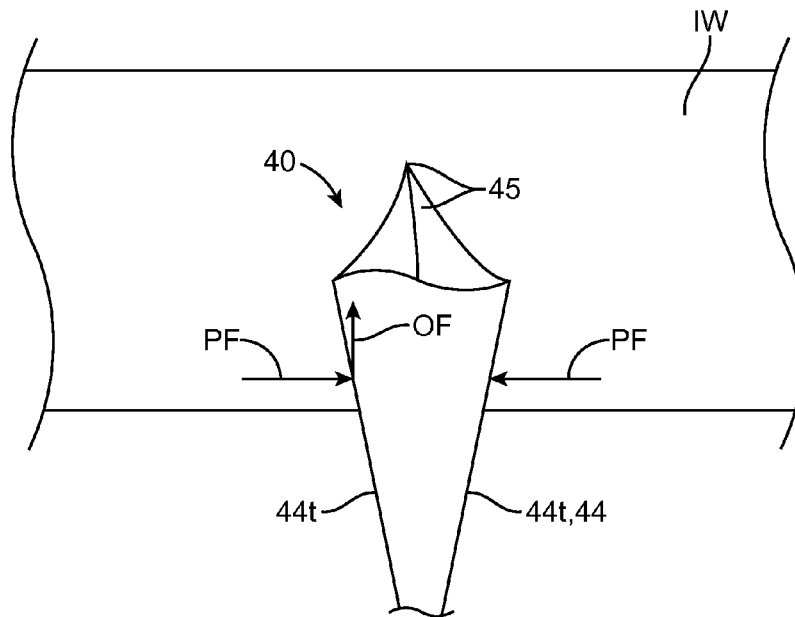


FIG. 8c

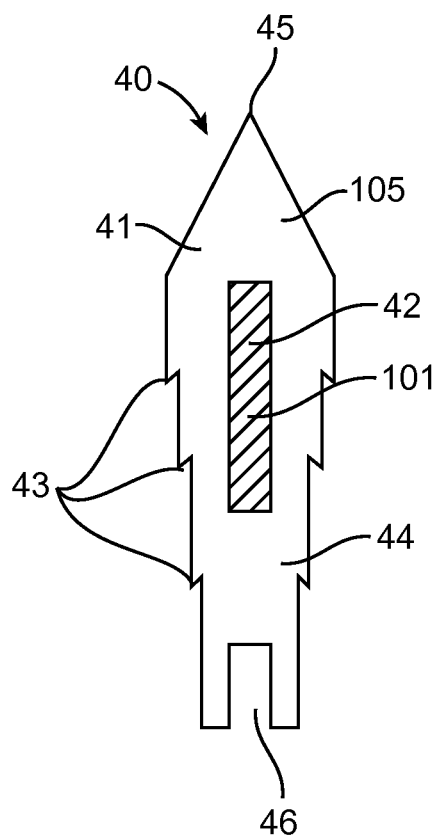


FIG. 8d

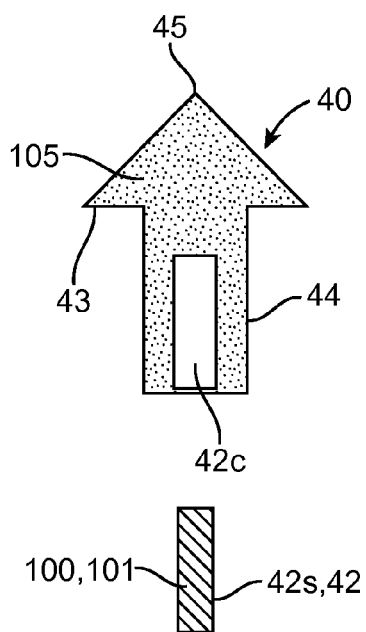


FIG. 8e

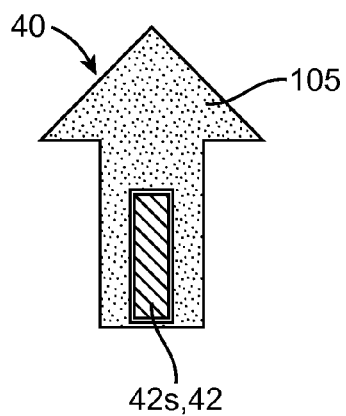


FIG. 8f

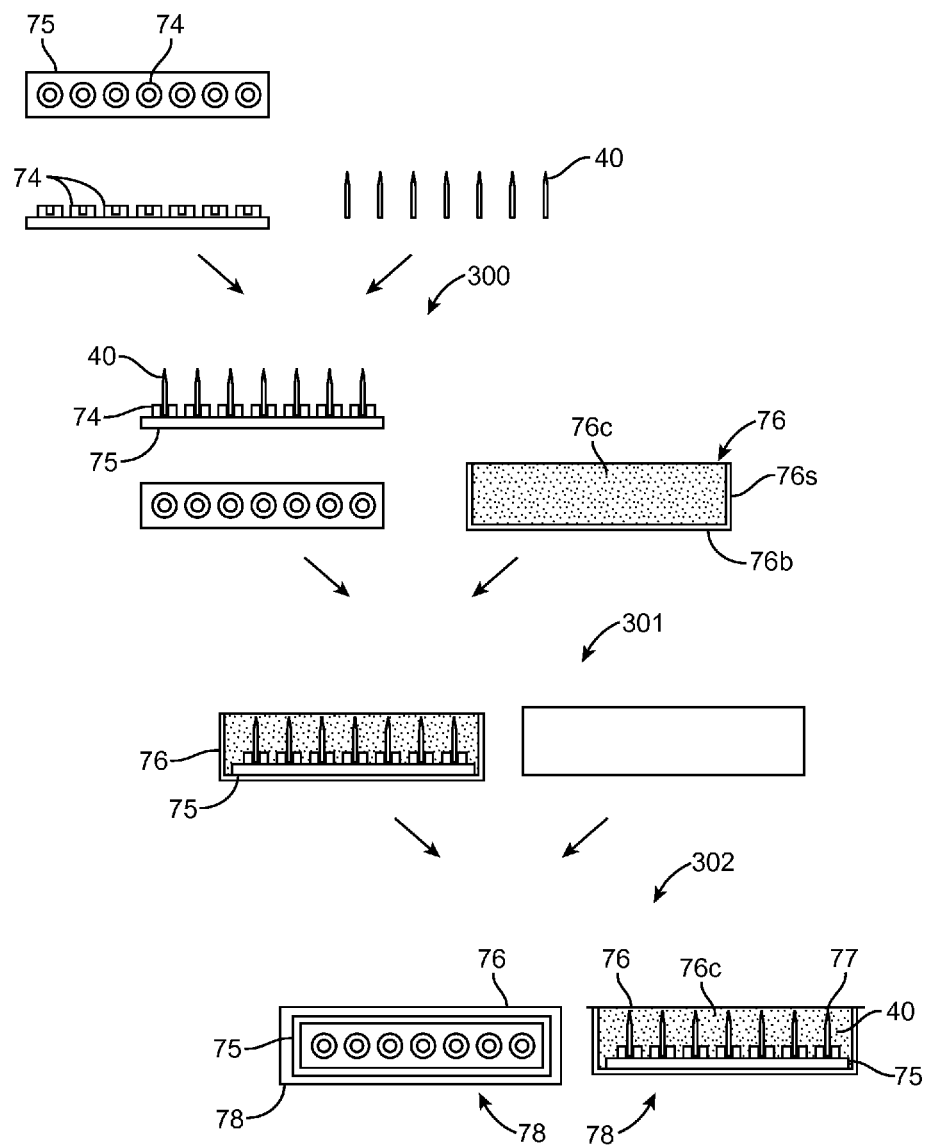


FIG. 9

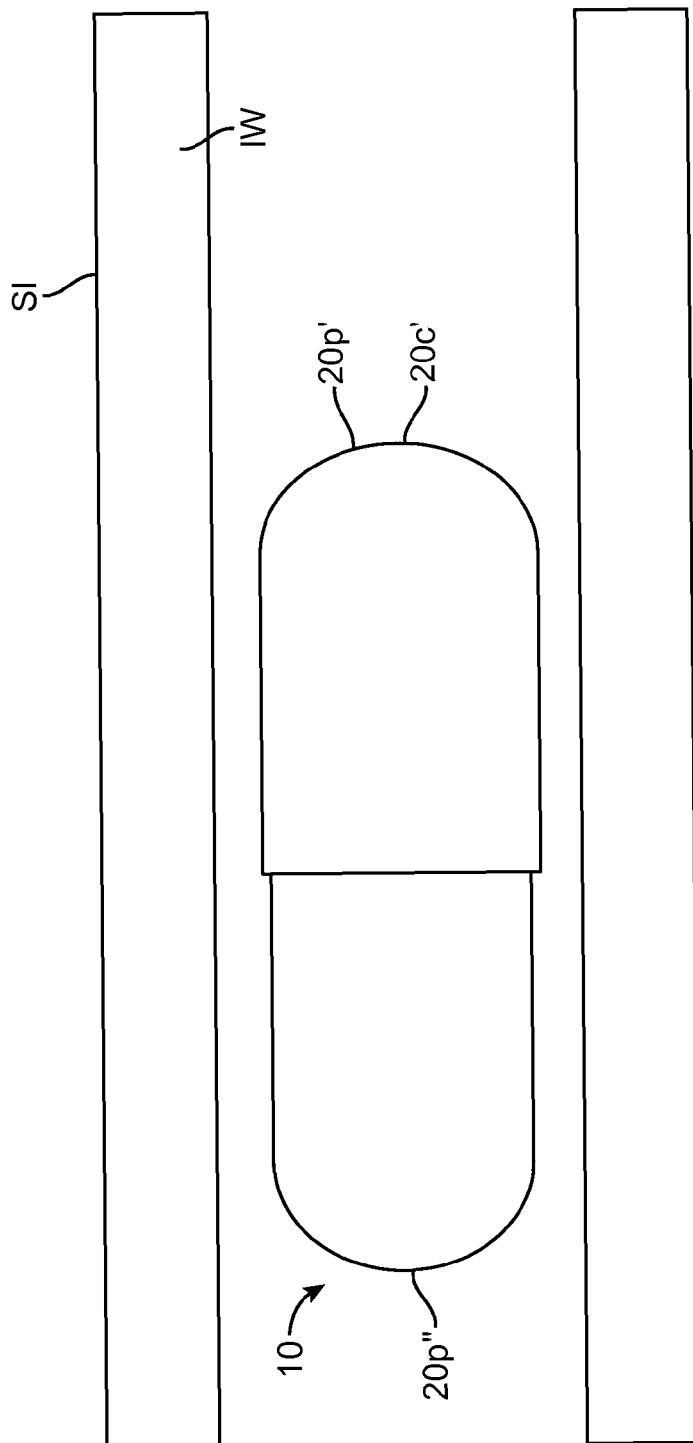


FIG. 10a

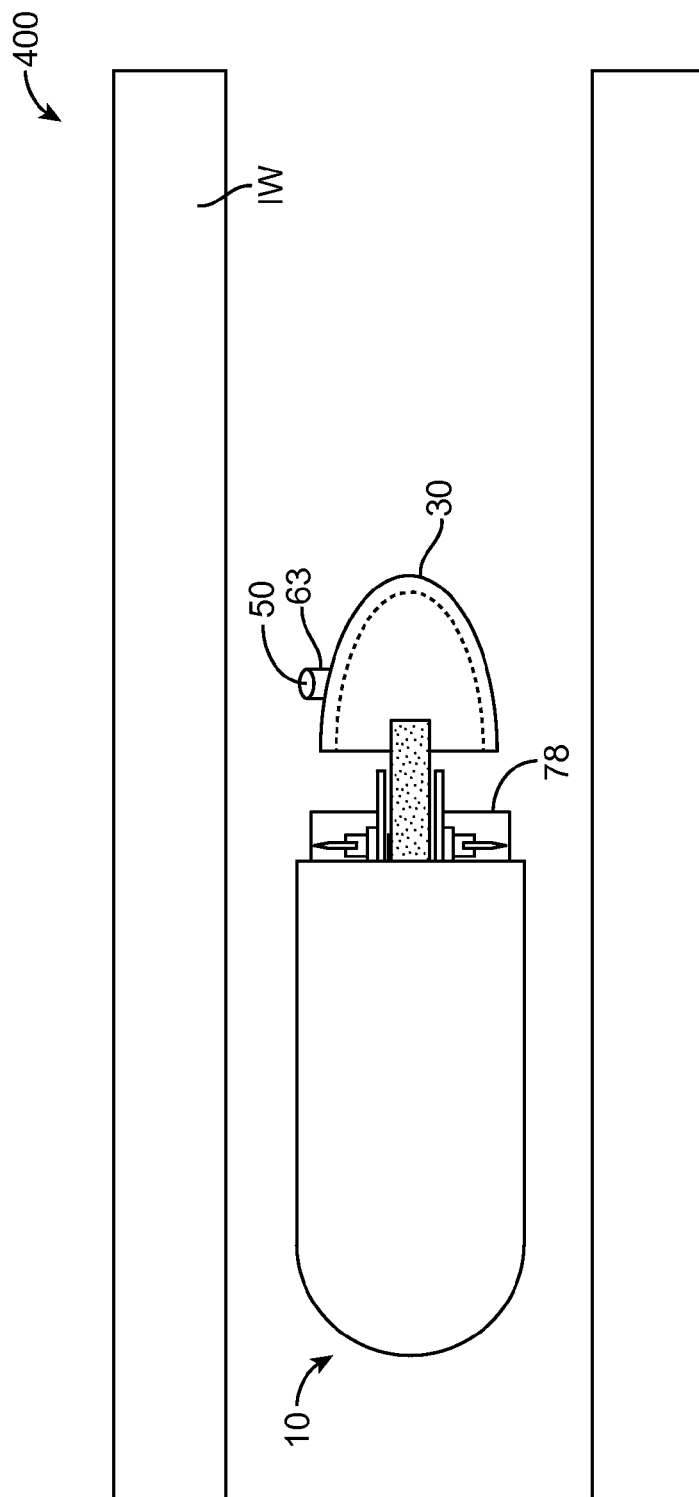


FIG. 10b

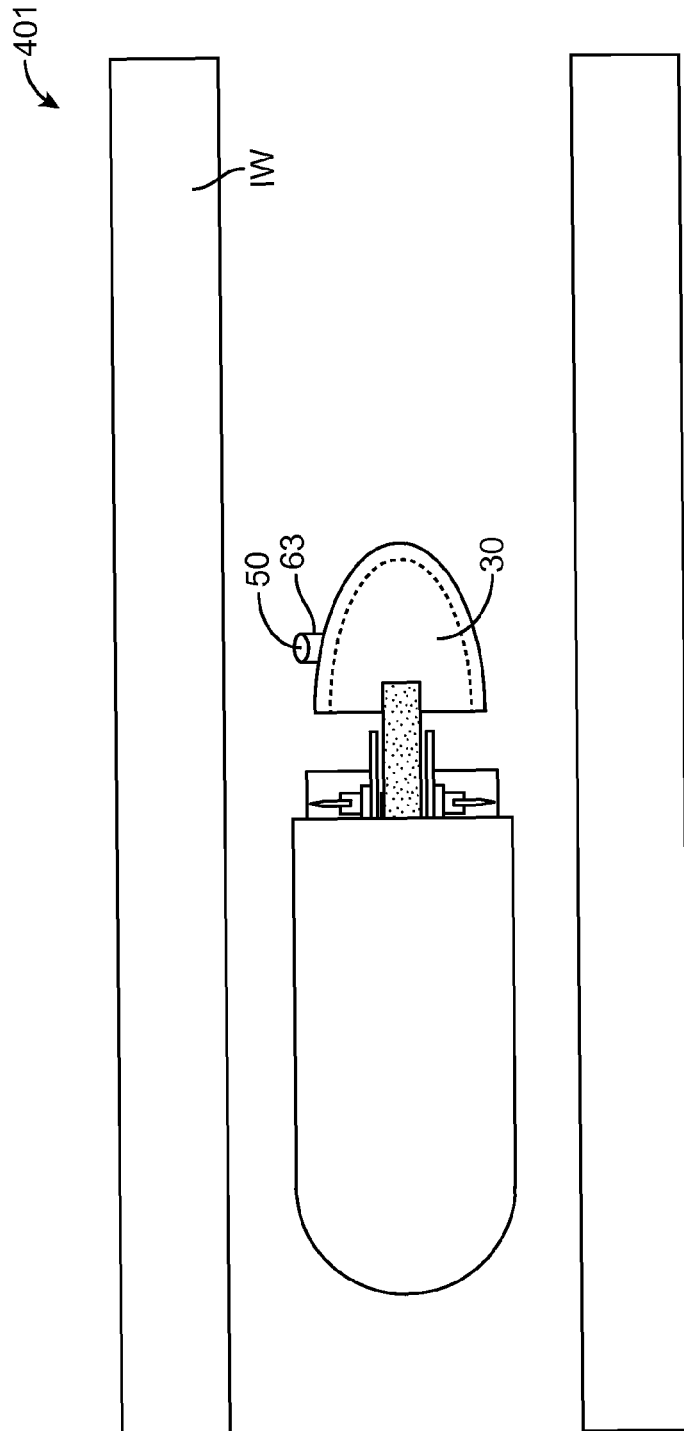


FIG. 10c

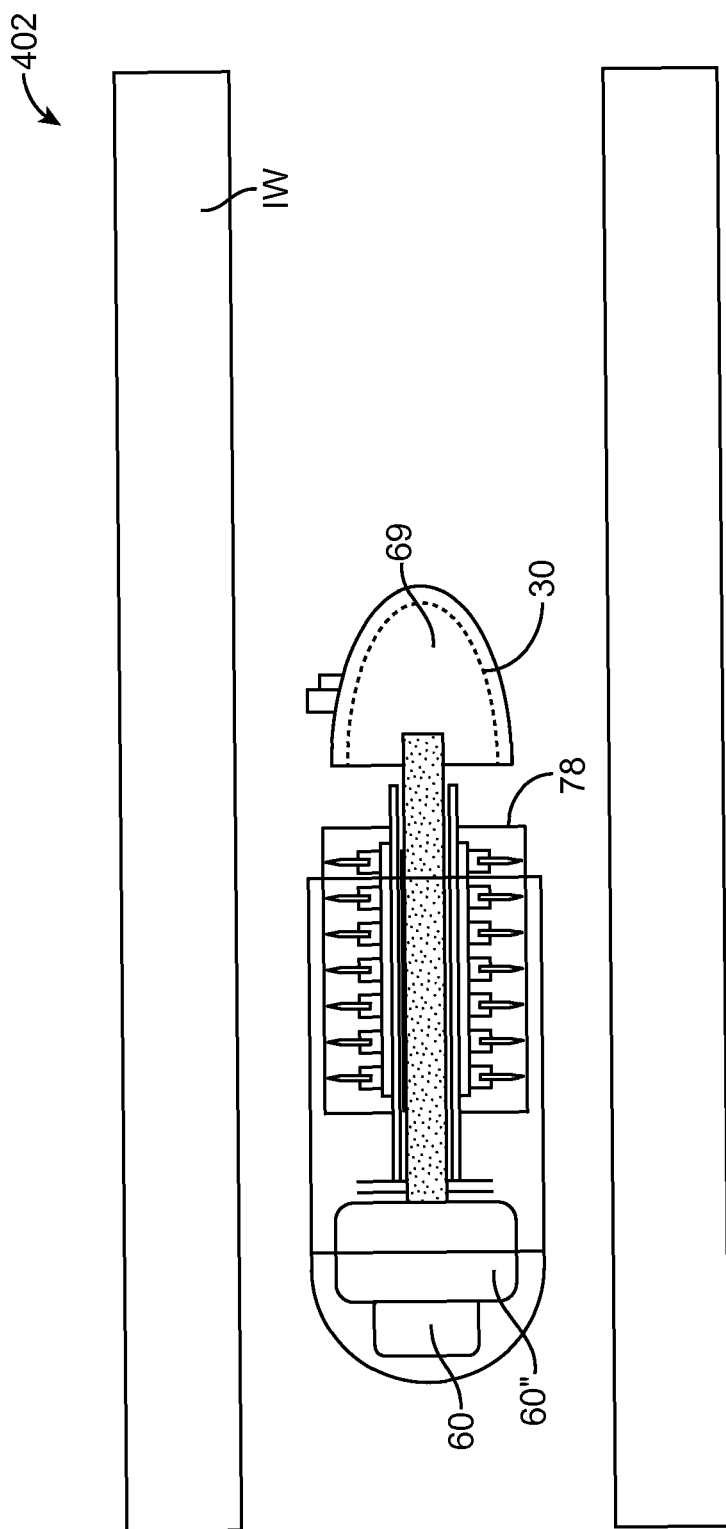


FIG. 10d

403

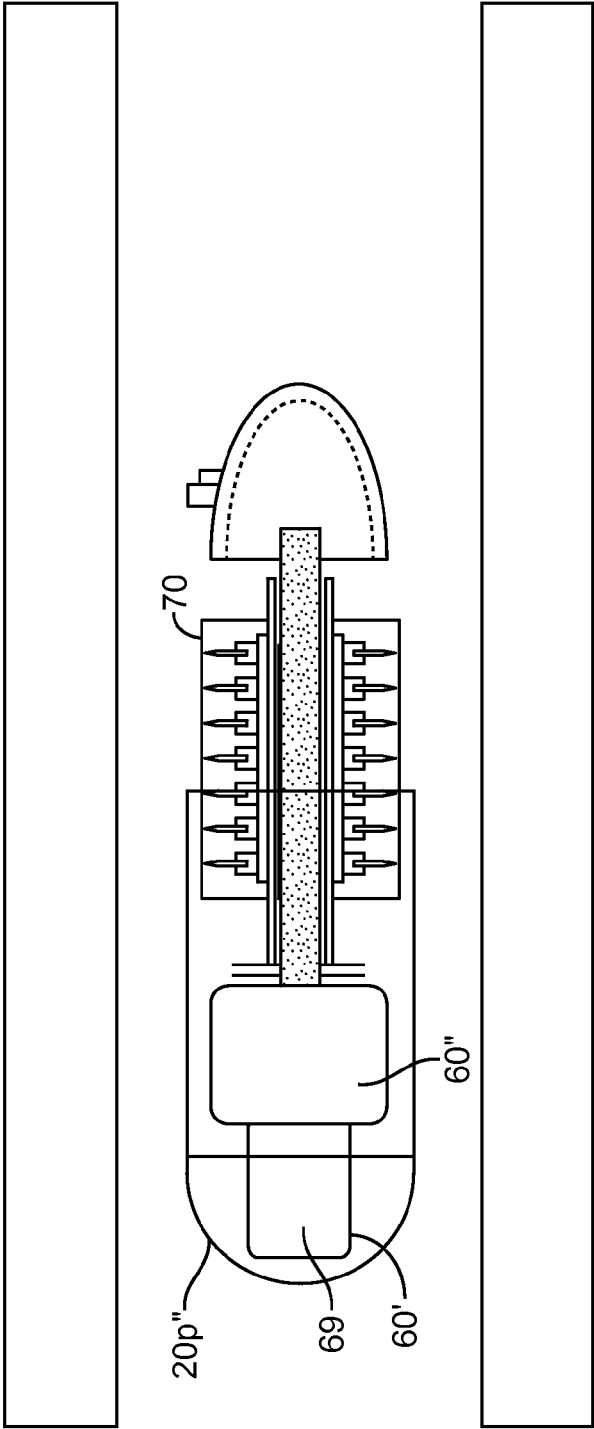


FIG. 10e

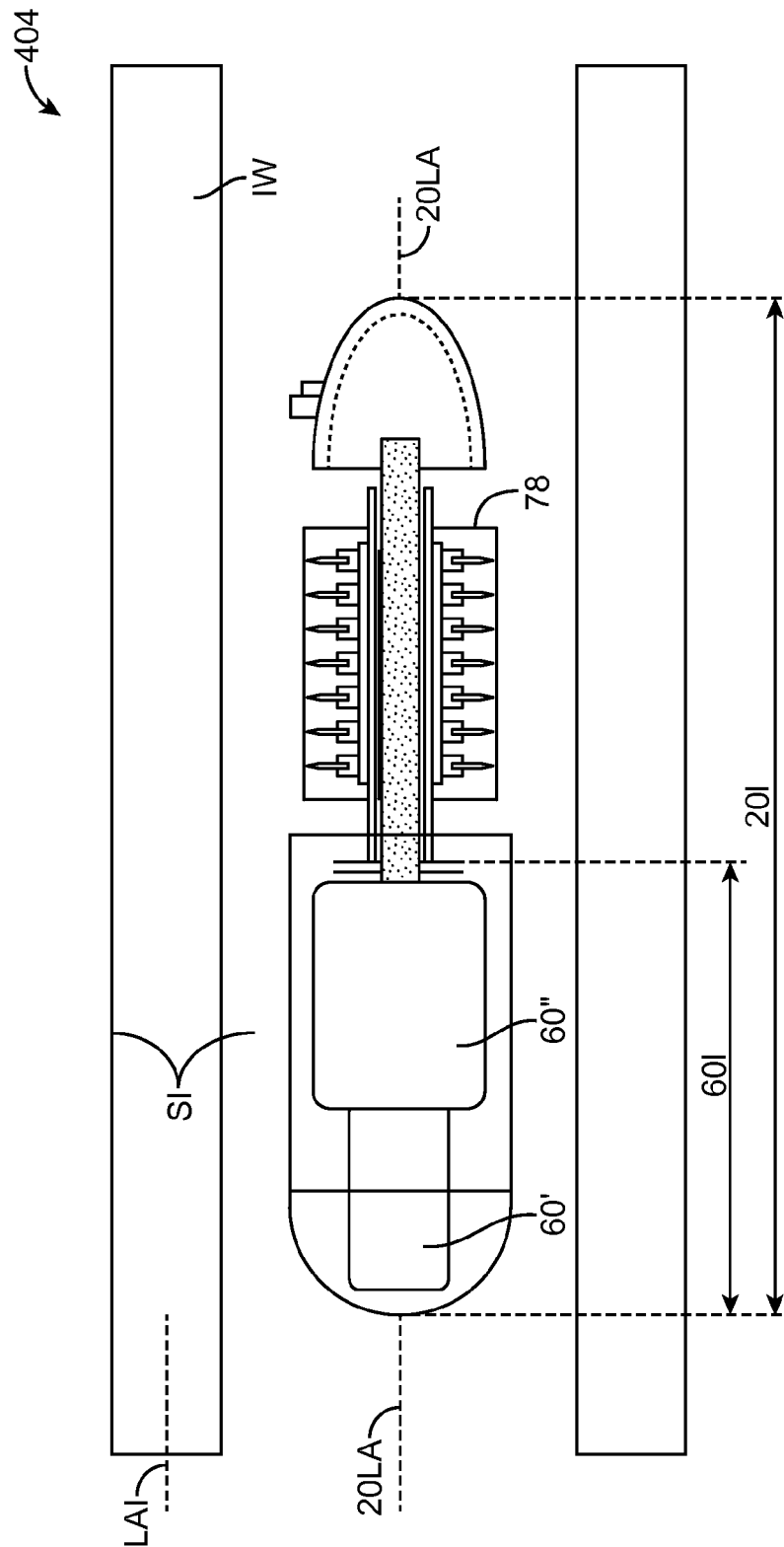


FIG. 10f

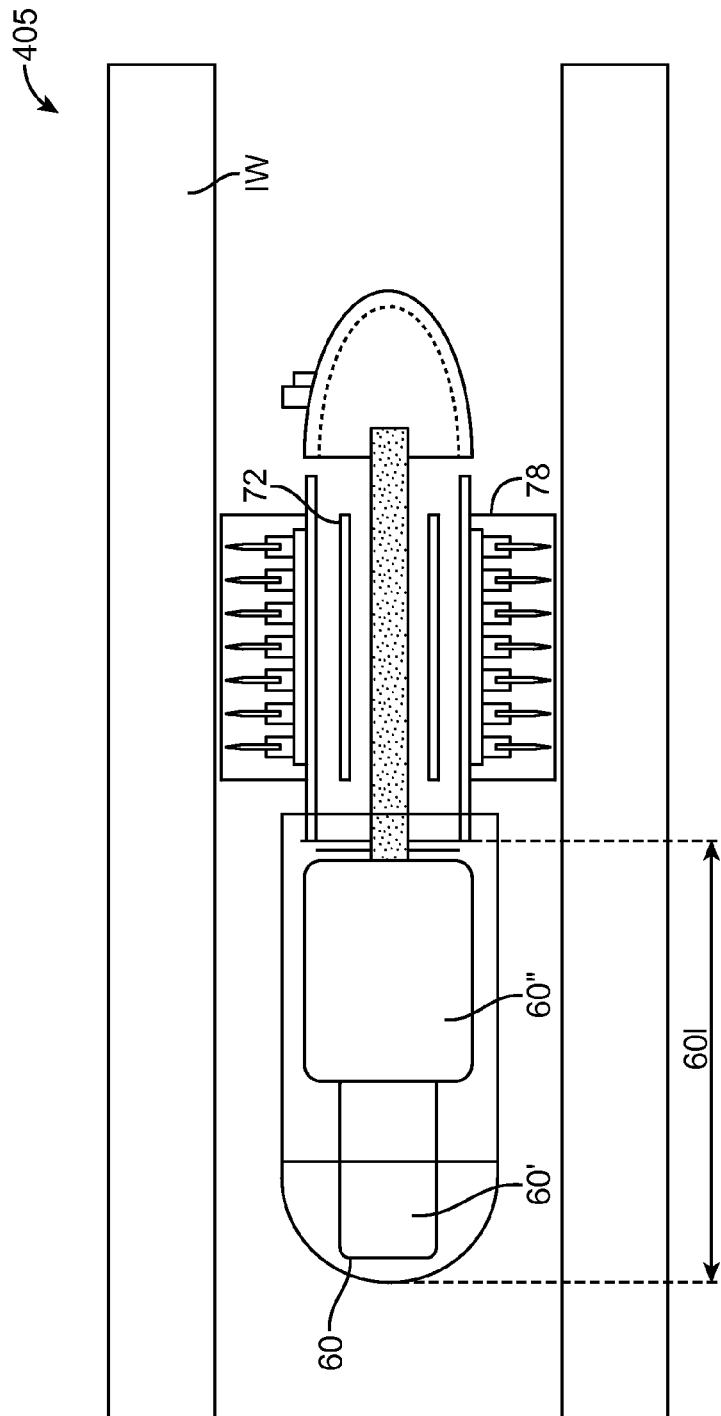


FIG. 10g

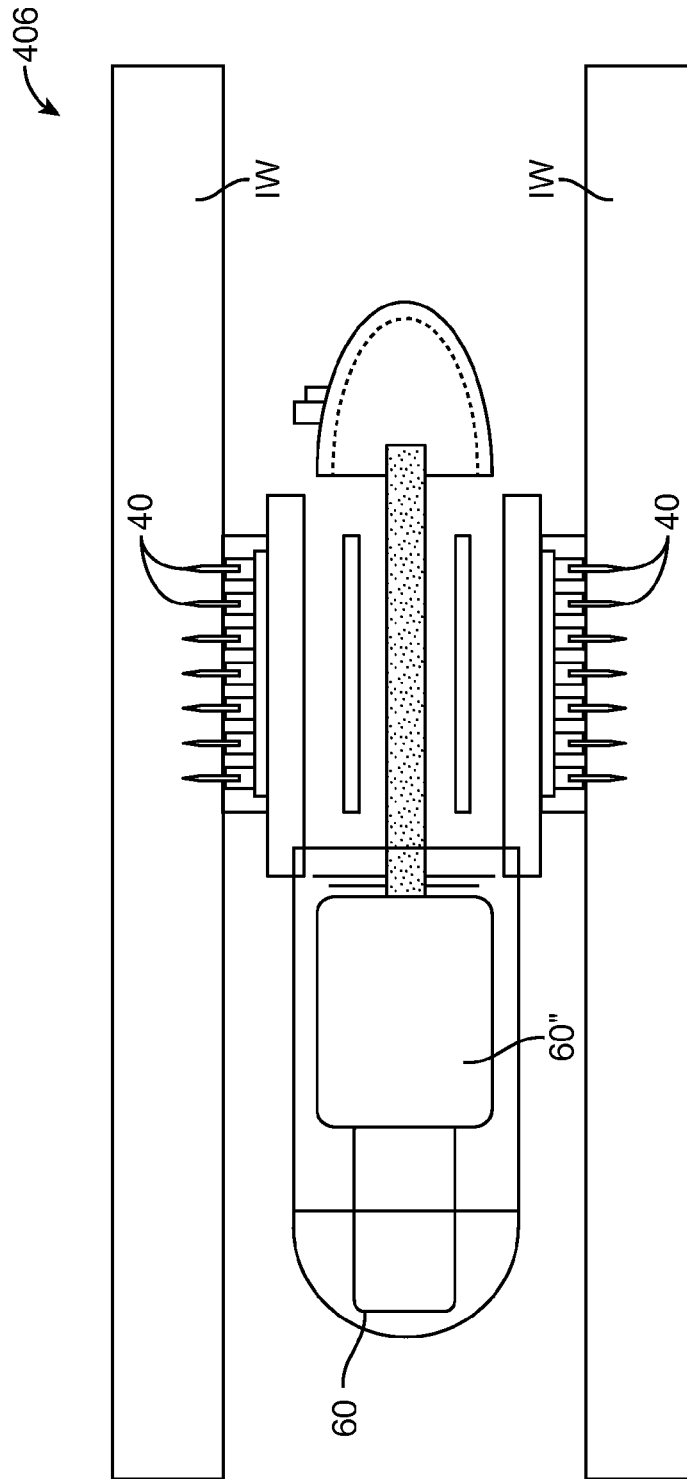


FIG. 10h

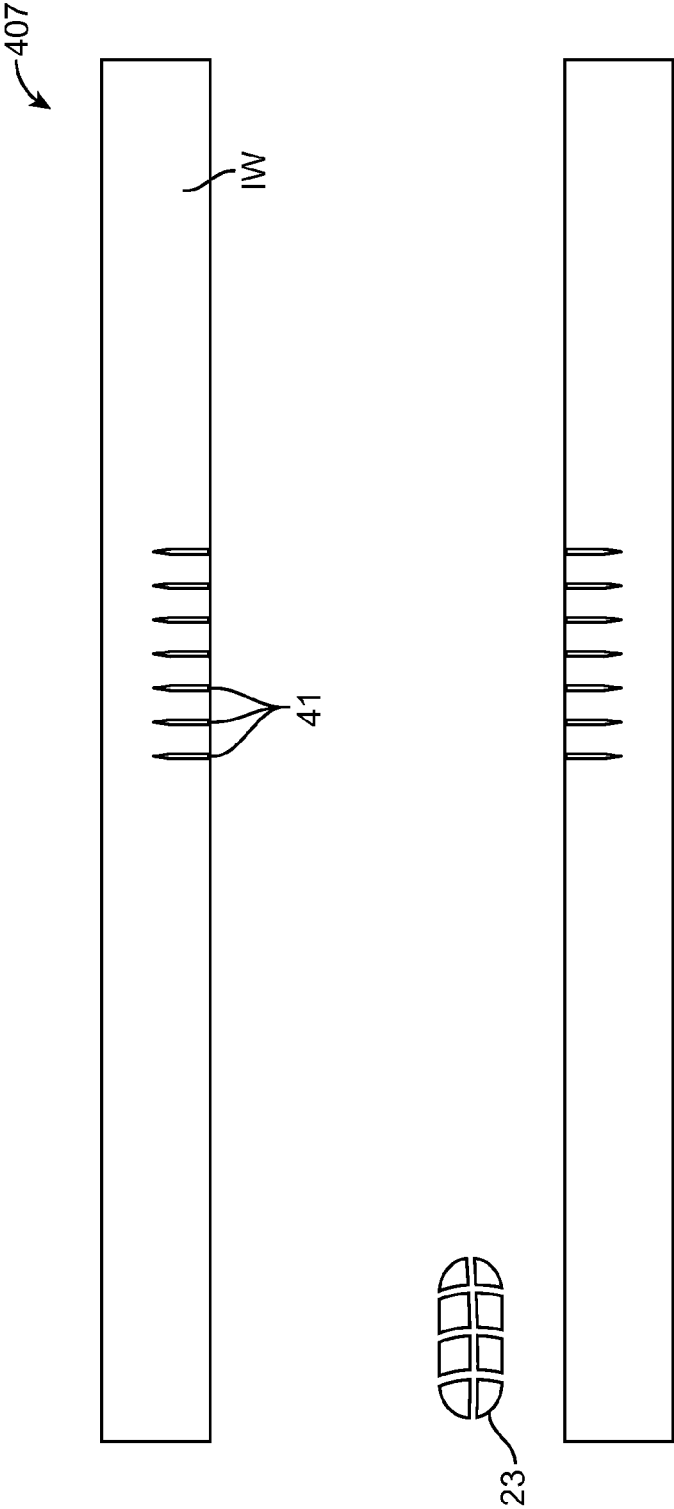


FIG. 10I

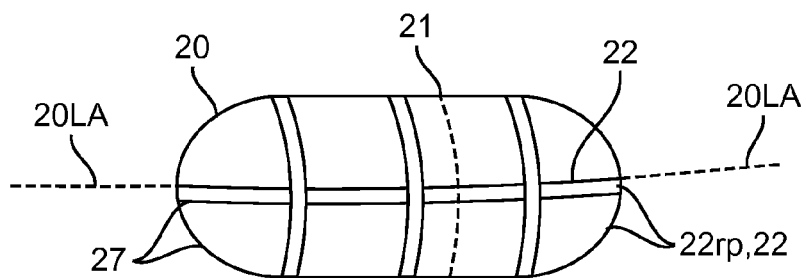


FIG. 11a

↓  
Deglutition

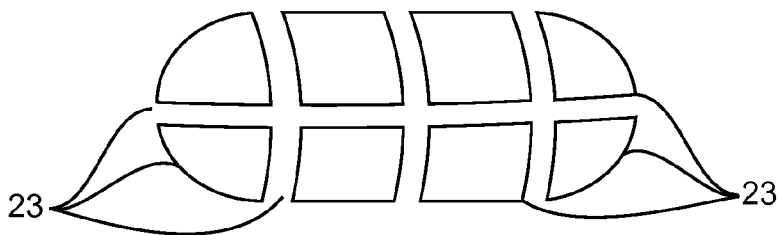


FIG. 11b

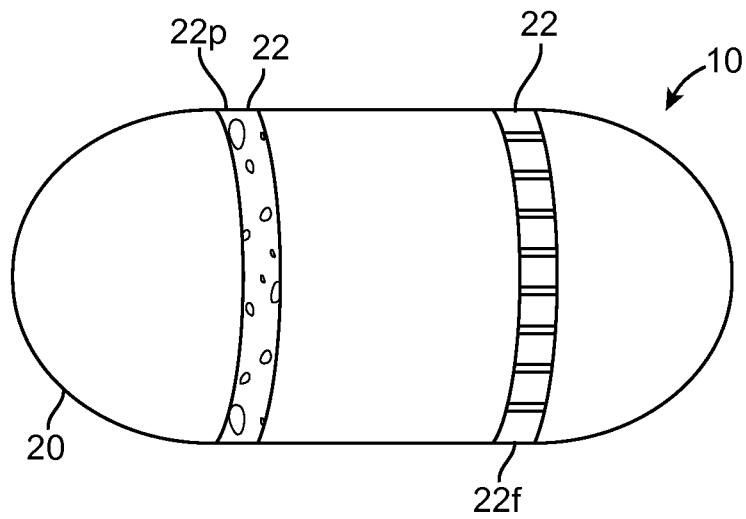
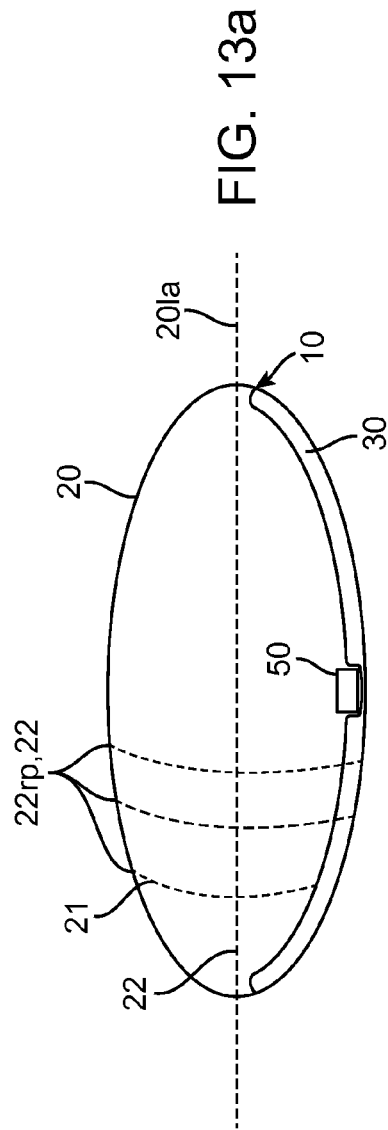
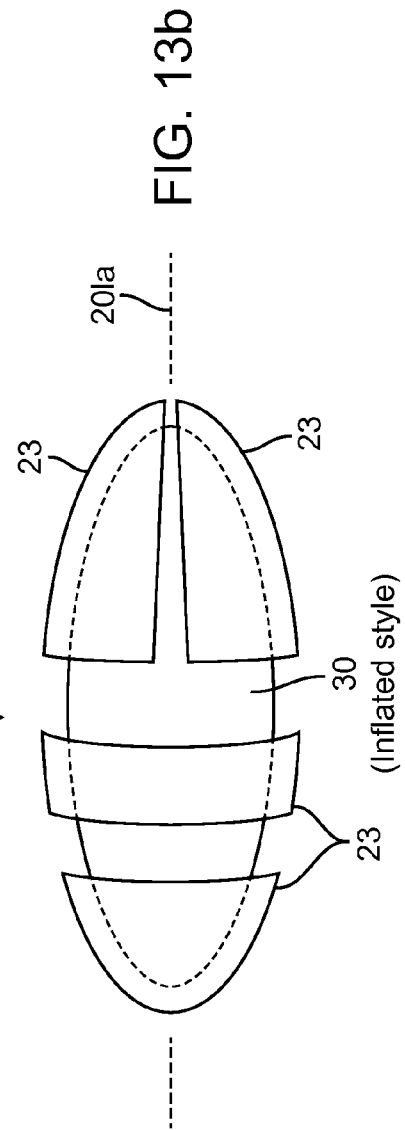


FIG. 12



Balloon inflation



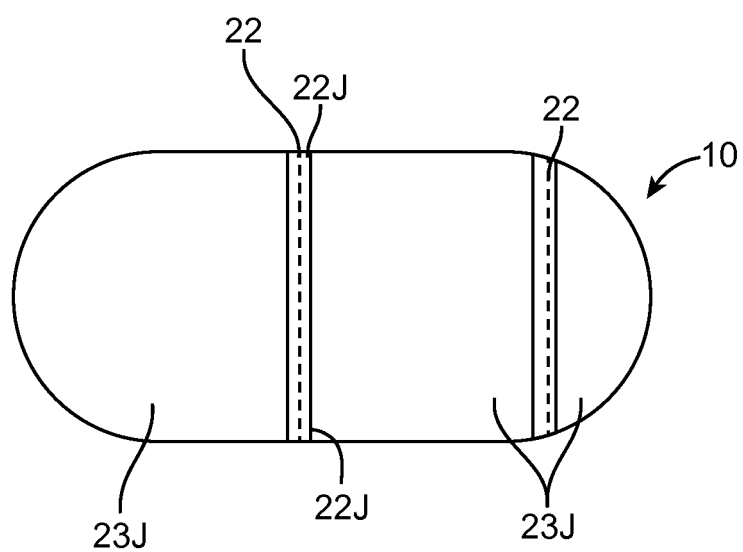


FIG. 14

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## DEVICE, SYSTEM AND METHODS FOR THE ORAL DELIVERY OF THERAPEUTIC COMPOUNDS

### CROSS-REFERENCE TO RELATED APPLICATIONS

This application claims the benefit of priority of Provisional U.S. Patent Application Ser. No. 61/571,641, entitled "Device, System and Methods for the Oral Delivery of Therapeutic Compounds", filed Jun. 29, 2011; which is fully incorporated by reference herein for all purposes.

This application is also a continuation-in-part of the following U.S. Patent Application Nos., both entitled "Swallowable Drug Delivery Device and Methods of Drug Delivery" and both filed on Dec. 23, 2010: application Ser. No. 12/978,233, now U.S. Pat. No. 8,721,620 and application Ser. No. 12/978,301 (now U.S. Pat. No. 8,562,589); the contents of both of which are hereby incorporated by reference for all purposes.

### BACKGROUND OF THE INVENTION

Embodiments of the invention relate to swallowable drug delivery devices. More specifically, embodiments of the invention relate to swallowable delivery devices for delivering therapeutic agents to the small intestine.

While there has been an increasing development of new drugs in recent years for the treatment of a variety of diseases, many including proteins, antibodies and peptides have limited application because they cannot be given orally. This is due to a number of reasons including: poor oral toleration with complications including gastric irritation and bleeding; breakdown/degradation of the drug compounds in the stomach; and poor, slow or erratic absorption of the drug. Conventional alternative drug delivery methods such as intravenous and intramuscular delivery have a number of drawbacks including pain and risk of infection from a needle stick, requirements for the use of sterile technique and the requirement and associated risks of maintaining an IV line in a patient for an extended period of time. While other drug delivery approaches have been employed such as implantable drug delivery pumps, these approaches require the semi-permanent implantation of a device and can still have many of the limitations of IV delivery. Thus, there is a need for an improved method for delivery of drugs and other therapeutic agents.

### BRIEF SUMMARY OF THE INVENTION

Embodiments provide devices, systems, kits and methods for delivering drugs and other therapeutic agents to various locations in the body. Many embodiments provide a swallowable device for delivering drugs and other therapeutic agents within the GI tract. Particular embodiments provide a swallowable device such as a capsule for delivering drugs and other therapeutic agents into the wall of the small intestine, large intestine or other GI organ wall. Embodiments of the invention are particularly useful for the delivery of drugs and other therapeutic agents which are poorly absorbed, poorly tolerated and/or degraded within the GI tract. Further, embodiments of the invention can be used to deliver drugs and other therapeutics such as proteins, polypeptides and antibodies which were previously only capable of or preferably delivered by intravenous or other form of parenteral administration (e.g., intramuscular, etc.). Additionally,

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embodiments of the invention are useful for achieving rapid release of a drug into the blood stream via oral delivery.

In one aspect, a swallowable device is provided for delivering drugs or other therapeutic agent into the wall of the small or large intestine or other organ of the gastro-intestinal tract organ. The device comprises a capsule sized to be swallowed and pass through the gastro-intestinal tract, a deployable aligner positioned within the capsule for aligning a longitudinal axis of the capsule with the a longitudinal axis of the small intestine, a delivery mechanism for delivering the therapeutic agent into the intestinal wall and a deployment member for deploying at least one of the aligner or the delivery mechanism. The capsule wall is degradable by contact with liquids in the GI tract but also may include an outer coating or layer which only degrades in the higher pH's found in the small intestine, and serves to protect the underlying capsule wall from degradation within the stomach before the capsule reaches the small intestine at which point the drug delivery is initiated by degradation of the coating. In use, such materials allow for the targeted delivery of a therapeutic agent in a selected portion of the intestinal tract such as the small intestine. Suitable outer coatings can include various enteric coatings such as various co-polymers of Methacrylic Acid and Ethyl Acrylate.

In many embodiments, the capsule is formed from two portions such as a body and a cap, where the cap which fits onto the body, e.g., by fitting sliding over or under the body. One portion such as the cap can be configured to degrade above a first pH (e.g., pH 5.5) and the second portion can be configured to degrade above a second higher pH (e.g. 6.5). This allows for triggers and/or mechanisms in one portion of the capsule to be actuated before those in the other portion of the capsule because intestinal fluids will first enter those portions where the lower pH coating has degraded thus actuating triggers which are responsive to such fluids (e.g., degradable valves). In use, such embodiments provides several benefits to the drug delivery process including an enhanced degree of locational specificity for drug delivery and improved reliability for such delivery. This is due to the fact that deployment of a particular sub-mechanism, such as the aligner, can begin in the upper area of the small intestine SI allowing the capsule to be aligned within the intestine for optimal delivery as well as allowing sufficient time for deployment/actuation of other mechanisms to achieve drug delivery into the intestinal wall while the capsule is still in the small intestine or other selected location.

In addition to having degradable cap and body section, selectable portions of the capsule can be configured to allow the entire device to controllably degrade into smaller pieces. Such embodiments facilitate passage and excretion of the devices through GI tract. In particular embodiments, the capsule can include seams of biodegradable material which controllably degrade to produce capsule pieces of a selectable size and shape to facilitate passage through the GI tract. The seams can be pre-stressed, perforated or otherwise treated to accelerate degradation. The seams can also be so treated so to allow the capsule to be broken apart into smaller pieces by the forces applied from expansion of the balloon or other expandable member. In other embodiments for producing capsule degradation after deployment of the tissue penetrating members, the capsule can be comprise two halves or other fractional sections which are mechanically fit together, e.g., by a snap fit and thus readily separated by the forces applied from balloon inflation.

The aligner will typically comprise an expandable balloon known as an aligning balloon which can be fabricated from various polymers known in the medical device arts. The align-

ing balloon serves to extend the length of the capsule when the aligning balloon is inflated such that the capsule aligns in a parallel fashion with the longitudinal axis of the small intestine. Further, the aligning balloon can have an inflated shape and length such that when inflated, forces exerted by the peristaltic contractions of the intestine on the extended capsule serve to align the capsule in a parallel fashion with the longitudinal axis of the small intestine. Suitable shapes can include an elongated hotdog like shape. Suitable lengths can include a range between about  $\frac{1}{2}$  to two times the length of the capsule. For embodiments where the deployment engine includes use of a deploying balloon and chemical reactants, the aligning balloon is fluidically coupled to the deployment balloon such that expansion of the deploying balloon serves to expand the aligning balloon. In some embodiments, the aligning balloon can contain the chemical reactants which react upon mixture with water or other liquid from the deploying balloon. In addition to performing an alignment function, inflation of the aligning balloon can also serve to push out various components of the device contained within capsule such as the delivery. In use, such configurations improve the reliability for delivery of the therapeutic agent since it is not necessary to wait for particular portions of the capsule overlying the delivery mechanism to be degraded before drug delivery can occur.

In many embodiments, the deployment member will comprise an expandable balloon, known as the deployment balloon, that is fluidically coupled to the aligner balloon by means of a connector tube and a pH degradable valve which is responsive to the higher pH's found in the intestinal fluids. In the deployed state, the deployment balloon can have a dome shape which corresponds to the shape of an end of the capsule. In many embodiments, the deployment balloon in combination with the aligner balloon can comprise a deployment engine, where the deployment balloon contains liquid water and the aligner balloon contains at least one chemical reactant that reacts to produce a gas in the presence of water, which in turn expands the aligner balloon. The reactants will typically include at least two reactants for example, an acid such as citric acid and a base such as sodium hydroxide or potassium hydroxide, which can have about a 1:2 ratio, though other ratios are also contemplated. Other reactants including other acids, e.g., ascorbic acid and bases are also contemplated. When the valve or other separation means opens, the reactants mix in the liquid and produce a gas such as carbon dioxide which expands the aligner balloon or other expandable member.

In one alternative embodiment, the deployment balloon can actually comprise two balloons connected by a connecting tube or other connection means having a degradable valve that is pH responsive. The two balloons can each have a half dome shape allowing them to fit into the end portion of the capsule when in the expanded state. One balloon can contain the chemical reactant(s) (e.g., sodium bicarbonate, citric acid, etc.) and the other the liquid water, so that when the valve is degraded the two components mix to form a gas (e.g., carbon dioxide) which inflates both balloons/compartments and in turn, the aligning balloon. In these embodiments the deployment engine comprises the two deployment balloons. In yet another alternative embodiment, the deployment balloon can include at least a first and a second portion or compartment which are separated by a separation valve or other separation means. Water, can be disposed within the first compartment and the chemical reactants in the other. When the valve or other separation means opens, the reactants mix in the liquid and produce a gas which is used to expand the aligning balloon and the deployment balloon. In various embodiments

using chemical reactants, the chemical reactants alone in combination with the deployment balloon can comprise a deployment engine for deploying one or both of the aligning balloon (or other aligner) or the delivery mechanism. Other forms of a deployment engine are also contemplated such as use of expandable piezo-electric materials (that expand by application of a voltage), springs and other shape memory materials and various thermally expandable materials.

Various embodiments of the valve which separates the aligning balloon from the deployment balloon can be configured to open in a number of ways and responsive to a number of conditions. Typically, the valve will be configured to open by having one or more portions degrade in response to the higher pH found in intestinal fluids and may be fabricated from various enteric materials known in the art such as various co-polymers of methacrylic acid and co-ethyl acrylate described herein. In other embodiments, including those where the deployment balloon contains the chemical reactants, the valve can be configured to open in response to a selected pressure so as to allow the gas from the deployment balloon to inflate the aligning balloon. Similarly, the same or related embodiments of such a pressure sensitive valve can be used to provide for inflation of the delivery balloon upon the development of sufficient pressure in the aligning balloon so that a serial inflation effect is achieved. In an alternative or additional embodiment, the valve may also be configured to open in response to compressive forces applied by a peristaltic contraction within the small intestine. In still another approach, the valve may be a time release valve configured to open after a certain period of time after an activation step initiated by the patient such as the peeling of a tab or pressing of a button.

Embodiments of the delivery mechanism will typically comprise an expandable member such as an expandable balloon (known as the delivery balloon) that is fluidically coupled to the aligning balloon and a delivery assembly that is coupled to a wall of the delivery balloon. At least one tissue penetrating member (TPM) is coupled to the delivery device. In various embodiments, the delivery balloon can have an elongated shape with two relatively flat faces connected by an articulated accordion-like body. The flat faces can be configured to press against the intestinal wall upon expansion of the balloon so as to insert the TPM into the intestinal wall. TPM's can be positioned on one or both faces to allow insertion of drug containing TPMs on opposite sides of the intestinal wall. The faces may have sufficient surface area to allow for placement of a number of drug containing tissue penetrating members on each face.

The TPM contains the drug or other therapeutic agent and is configured to be inserted into the intestinal wall by expansion of the delivery balloon or other expandable delivery means. The TPM typically, comprises a shaft including a proximal portion detachably coupled to the delivery device, a tissue penetrating distal portion and a retaining feature for retaining the tissue penetrating member within the intestinal wall. However, in some embodiments the TPM need not include the retaining feature, but instead can have shape or otherwise be configured to be retained in the intestinal wall without the retaining feature. The TPM is described in further detail below.

In many embodiments, the delivery mechanism device comprises a delivery structure coupled to delivery balloon or other expandable deploying member. In one embodiment, the delivery structure has an open box structure including side walls and a bottom wall which collectively defines a cavity. The delivery balloon or other delivery member may include multiple carrying structures so as to place TPMs on multiple

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locations of the intestinal wall. In embodiments of the delivery balloon having an accordion-like shape on or more carrying structures can be placed on each of face of the delivery balloon. The carrying structure can have a unitary construction and may be fabricated using vacuum forming. The bottom wall is attached to the expandable member for example by an adhesive. An advancement structure is positioned in the cavity and includes one or more tissue penetrating members detachably coupled to the advancement structure. A protective penetrable film is coupled to the side walls and covering the cavity. The protective film seals the tissue penetrating members inside the advancement structure and serves as a protective barrier for the tpm to protect them from exposure to humidity and oxidation. In use, this film provides an additional level of protection for preventing the therapeutic agent from being degraded within the intestinal tract before it is delivered into the intestinal wall. The film also serves to extend the shelf life of the therapeutic agent preparation by protecting the preparation from exposure to moisture and oxidation.

The TPM is formed at least in part from a therapeutic agent preparation including a drug or other therapeutic agent that is configured to dissolve or otherwise be absorbed within the intestinal wall so as to deliver the therapeutic agent preparation to the patient's blood stream. The therapeutic agent preparation may also include one or more pharmaceutical excipients known in the art, e.g., disintegrants, binders etc. The TPM is desirably configured to penetrate a selected distance into the intestinal wall so as to deliver therapeutic agent to a particular tissue layer of the intestinal wall, for example the mucosal layer, submucosal layer, etc. This can be achieved through the use of stops positioned on the TPM shaft and/or configuring the TPM shaft to bend or even shear once it penetrates a selected distance in the intestinal wall.

Typically, the drug or other therapeutic agent delivered by the TPM will be mixed in with a biodegradable polymer such as PGLA and/or a sugar such as maltose. In such embodiments, the TPM may comprise a substantially heterogeneous mixture of drug and biodegradable polymer. Alternatively, the penetrating member may include a portion formed substantially from biodegradable polymer and a separate section or compartment that is formed from or contains the drug or other therapeutic agent. For example, in one embodiment the TPM may comprise an outer shell of biodegradable material with a hollow core which is fitted with a slug (e.g., cylinder shaped) of the therapeutic agent. The tip or tissue penetrating portion of the TPM can include a harder material such as a sugar so as to be able to readily penetrate tissue. Once placed in intestinal wall, the tissue penetrating member is degraded by the interstitial fluids within the wall tissue, the drug dissolves in those fluids and is absorbed into the blood stream by the capillaries in or around the intestinal wall tissue. The TPM will also typically include one or more tissue retaining features such as a barb or hook to retain the penetrating member within the tissue of the intestinal wall after advancement. The retaining features can be arranged in various patterns to enhance tissue retention such as two or more barbs symmetrically distributed around the member shaft. However, the TPM can also be retained in the intestinal through other means such as by a reverse taper or other shape. The reverse taper shape may also be combined with one or more retaining features to further enhance retention.

The drug or other therapeutic agent can be in solid form and then formed into the shape of the tissue penetrating member using molding or other like method or may be in solid or liquid form and then added to the biodegradable polymer in liquid form with the mixture then formed into the tpm using molding or other forming method known in the polymer arts.

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Desirably, embodiments of the tissue penetrating member comprising a drug and degradable polymer are formed (e.g., cured) at temperatures which do not produce any substantial thermal degradation of the drug including drugs such as various peptides and proteins. This can be achieved through the use of room-temperature curing polymers and room temperature molding and solvent evaporation techniques known in the art. In particular embodiments, the amount of thermally degraded drug within the tissue penetrating member is desirably less than about 10% by weight, more preferably less than 5% and still more preferably, less than 1%. The thermal degradation temperatures for a particular drug are known or can be determined using methods known in the art and then this temperature can be used to select and adjust the particular polymer processing methods (e.g., molding, curing, solvent evaporation etc.).

For various embodiments of the invention wherein one or more of the aligner, deployment member, delivery member comprises an expandable balloon, the balloon can have material properties and dimensions (e.g., wall thickness) allowing the balloon to be wrapped (or otherwise disposed in the capsule) so as to occupy reduced/minimal space. Accordingly, various embodiments of expandable balloons used by the invention can be thin walled e.g., less than about 0.001 inches and can comprise various non compliant polymers known in the art such as PET, polyethylene and polyimide.

One or more embodiments of the expandable balloons will also typically include a deflation valve which serves to deflate the balloon after inflation. The Deflation valve can comprise biodegradable materials which are configured to degrade upon exposure to the fluids in the small intestine and/or liquid in one of the compartments of the balloon so as to create an opening or channel for escape of gas within balloon. In particular embodiments, the deflation valve comprises a tube valve attached to the end of the delivery balloon (opposite to the end which is coupled to the aligner balloon). The tube valve comprises a hollow tube having an end portion filled with a material such as maltose that degrades upon exposure to fluid such as the fluid in the small intestine. The positioning of the obstructing material in the tube valve is configured to provide sufficient time for the delivery balloon to inflate and deliver the tissue penetrating members into the intestinal wall before the obstructing material dissolves to open the tube valve. According to one or more embodiments, once the deflation valve opens, it not only serves to deflate the delivery balloon but also the aligner balloon and deployment balloon since in many embodiments, all three are fluidically connected. Opening of the deflation valve can be facilitated by placing it on the end of the delivery balloon that is forced out of the capsule by inflation of the aligner balloon so that it has good exposure to liquids in the small intestine. Similar tube deflation valves can also be positioned on one or both of aligner balloon and the deployment balloon. In these later two cases, the obstructing material in the tube valve can be configured to degrade over a time period to allow sufficient time for inflation of the delivery balloon.

Additionally, as further backup for insuring balloon deflation, one or more puncture elements can be attached to the inside surface of the capsule wall such that when one or more balloons used in embodiments of the invention fully inflate they contact and be punctured by the puncture element. In another alternative or additional embodiment of a means for deflation of the delivery balloon, one or more of the tissue penetrating members can be directly coupled to the delivery balloon and are configured to tear away from the balloon when they detach, tearing the balloon wall in the process. In

yet another alternative one or more tissue penetrating members on the delivery assembly and/or otherwise attached to the delivery balloon can be configured to puncture one or both of the delivery balloon and the aligner balloon upon inflation of the delivery balloon.

Another aspect of the inventions provides therapeutic agent preparations for delivery into the wall of the small intestine (or other wall of a lumen in the intestinal tract) using embodiments of the swallowable device described herein. The preparation comprises a therapeutically effective dose of at least one therapeutic agent (e.g., insulin, incretin, an anti-seizure compound, NSAIDs, an antibiotic etc). The preparation may comprise a solid, liquid, gel and combinations thereof and can include one or more pharmaceutical excipients. The preparation has a shape and material consistency to be contained in the swallowable capsule, delivered from the capsule into the lumen wall and degrade within the lumen wall to release the dose of therapeutic agent. Typically, this shape and material consistency are achieved by placing or forming the preparation into one or more embodiments of the tissue penetrating members described herein. The preparation may also have a selectable surface area to volume ratio so as enhance or otherwise control the rate of degradation of the preparation in the wall of the small intestine or other body lumen. The dose of the drug or other therapeutic agent in the preparation can be titrated downward from that which would be required for conventional oral delivery methods so that potential side effects from the drug can be reduced.

Another aspect of the invention provides methods for the delivery of drugs and the therapeutic agents into the walls of the GI tract using embodiments of the swallowable drug delivery devices. Such methods can be used for the delivery of therapeutically effective amounts of a variety of drugs and other therapeutic agents. These include a number of large molecule peptides and proteins which would otherwise require injection due to chemical breakdown in the stomach e.g., growth hormone, parathyroid hormone, insulin, interferons (for treatment of MS and other conditions) and other like compounds. Suitable drugs and other therapeutic agents which can be delivered by embodiments of invention include various antibodies (e.g., HER 2 antibodies), chemotherapeutic agents (e.g., interferon), insulin and related compounds for treating diabetes, glucagon like peptides (e.g., GLP-1, exenatide), parathyroid hormones, growth hormones (e.g., IFG and other growth factors), immune suppression agents (e.g., cyclosporines, cortisones, etc), vaccines and anti parasitic agents such as various anti malarial agents. In specific embodiments, embodiments of the swallowable capsule can be used to delivery therapeutically effective amounts of the monoclonal antibody adalimumab for the treatment of various autoimmune related disorders such as rheumatoid arthritis. The dosage of this or particular therapeutic agent can be titrated for the patient's weight, age, condition or other parameter.

In various method embodiments of the invention, embodiments of the swallowable drug delivery device can be used to deliver a plurality of drugs for the treatment of multiple conditions or for the treatment of a particular condition (e.g., a mixture of protease inhibitors for treatment HIV AIDs). In use, such embodiments allow a patient to forgo the necessity of having to take multiple medications for a particular condition or conditions. Also, they provide a means for facilitating that a regimen of two or more drugs is delivered and absorbed into the small intestine and thus, the blood stream at about the same time. Due to differences in chemical makeup, molecular weight, etc, drugs can be absorbed through the intestinal wall at different rates, resulting in different phar-

macokinetic distribution curves. Embodiments of the invention address this issue by injecting the desired drug mixtures at about the same time. This in turn, improves the pharmacokinetics and thus, the efficacy of the selected mixture of drugs.

Further details of these and other embodiments and aspects of the invention are described more fully below, with reference to the attached drawing figures.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1a is a lateral viewing showing an embodiment of a swallowable drug delivery device.

FIG. 1b is a lateral viewing showing an embodiment of a system including a swallowable drug delivery device.

FIG. 1c is a lateral viewing showing an embodiment of a kit including a swallowable drug delivery device and a set of instructions for use.

FIG. 1d is a lateral viewing showing an embodiment of a swallowable drug delivery device including a drug reservoir.

FIG. 1e is a lateral viewing illustrating use of an embodiment of a swallowable drug delivery device including transit of device in the GI tract and operation of the device to deliver drug.

FIGS. 2a and 2b are lateral view illustrating an embodiment of a capsule for the swallowable drug delivery device including a cap and a body coated with pH sensitive biodegradable coatings, FIG. 2a shows the capsule in an unassembled state and FIG. 2b in an assembled state

FIGS. 3a and 3b illustrate embodiments of unfolded multi balloon assemblies containing a deployment balloon, an aligner balloon, a delivery balloon and assorted connecting tubes; FIG. 3a shows an embodiment of the assembly for a single dome configuration of the deployment balloon; and FIG. 3b shows an embodiment of the assembly for dual dome configuration of the deployment balloon; and.

FIG. 3c is a perspective views illustrating embodiments of a nested balloon configuration which can be used for one or more embodiments of the balloons described herein including the aligner balloon.

FIGS. 4a-4c are lateral views illustrating embodiments of a multi compartment deployment balloon; FIG. 4a shows the balloon in a non-inflated state with the separation valve closed; FIG. 4b shows the balloon with valve open and mixing of the chemical reactants; and FIG. 4c shows the balloon in an inflated state.

FIGS. 5a-5g are lateral views illustrating a method for folding of the multiple balloon assembly, the folding configuration in each figure applies to both single and dual dome configurations of the deployment balloon, with the exception that FIG. 5c, pertains to a folding step unique to dual dome configurations; and FIG. 5d, pertains to the final folding step unique to dual dome configurations; FIG. 5e, pertains to a folding step unique to single dome configurations; and FIGS. 5f and 5g are orthogonal views pertaining to the final folding step unique to single dome configurations.

FIGS. 6a and 6b are orthogonal views illustrating embodiments of the final folded multi balloon assembly with the attached delivery assembly.

FIGS. 7a and 7b are orthogonal transparent views illustrating embodiments of the final folded multi balloon assembly inserted into the capsule.

FIG. 8a is a side view of an embodiment of the tissue penetrating member.

FIG. 8b is a bottom view of an embodiment of the tissue penetrating member illustrating placement of the tissue retaining features.

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FIG. 8c is a side view of an embodiment of the tissue penetrating member having a trocar tip and inverted tapered shaft.

FIG. 8d is a side view of an embodiment of the tissue penetrating member having a separate drug containing section.

FIGS. 8e and 8f are side views showing assembly of an embodiment of a tissue penetrating member having a shaped drug containing section. FIG. 8e shows the tissue penetrating member and shaped drug section prior to assembly; and FIG. 8f after assembly.

FIG. 9 provides assorted views of the components and steps used to assemble an embodiment of the delivery assembly.

FIGS. 10a-10i provides assorted views illustrating a method of operation of swallowable device to deliver medication to the intestinal wall.

FIG. 11a shows an embodiment of a swallowable drug delivery device including a capsule having bio-degradable seams positioned to produce controlled degradation of the capsule in the GI tract.

FIG. 11b shows the embodiment of FIG. 11a after having been degraded in the GI tract into smaller pieces.

FIG. 12 shows an embodiment of a capsule having biodegradable seams including pores and/or perforations to accelerate biodegradation of the capsule.

FIGS. 13a-13b, show an embodiment of a capsule having tearable seams arranged in a radial or lateral pattern for tearing of the capsule by inflation of the expandable balloon; FIG. 13a shows the capsule prior to inflation and FIG. 13b shows the capsule broken into pieces by the inflation of the balloon.

FIG. 14 shows an embodiment of a balloon tearable capsule fabricated from separate portions joined by seams, which can be torn by inflation of the expandable balloon.

#### DETAILED DESCRIPTION OF THE INVENTION

Embodiments of the invention provide devices, systems and methods for delivering medications in to various locations in the body. As used herein, the term "medication" refers to a medicinal preparation in any form which can include drugs or other therapeutic agents as well as one or more pharmaceutical excipients. Many embodiments provide a swallowable device for delivering medication within the GI tract. Particular embodiments provide a swallowable device such as a capsule for delivering medications to the wall of the small intestine or other GI organ.

Referring now to FIGS. 1-9, an embodiment of a device 10 for the delivery of medication 100 to a delivery site DS in the gastro-intestinal (GI) tract, comprises a capsule 20 sized to be swallowed and pass through the intestinal tract, a deployment member 30, one or more tissue penetrating members 40 containing medication 100, a deployable aligner 60 and a delivery mechanism 70. The deployable aligner 60 is positioned within the capsule and configured to align the capsule with the intestine such as the small intestine. Typically, this will entail aligning a longitudinal axis of the capsule with a longitudinal axis of the intestine; however, other alignments are also contemplated. The delivery mechanism 70 is configured for delivering medication 100 into the intestinal wall and will typically include a delivery member 72 such as an expandable member. The deployment member 30 is configured for deploying at least one of the aligner 60 or the delivery mechanism 70. As will be described further herein, all or a portion of the capsule wall is degradable by contact with liquids in the GI tract so as to allow those liquids to trigger the delivery of medication 100 by device 10. As used herein, "GI tract" refers

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to the esophagus, stomach, small intestine, large intestine and anus, while "Intestinal tract" refers to the small and large intestine. Various embodiments of the invention can be configured and arranged for delivery of medication 100 into both the intestinal tract as well as the entire GI tract.

Device 10 including tissue penetrating member 40 can be configured for the delivery of liquid, semi-liquid or solid forms of medication 100 or combinations of all three. Whatever the form, medication 100 desirably has a material consistency allowing the medication to be advanced out of device 10, into the intestinal wall (small or large intestine) or other luminal wall in the GI tract and then degrade within the intestinal wall to release the drug or other therapeutic agent 101. The material consistency of medication 100 can include one or more of the hardness, porosity and solubility of the preparation (in body fluids). The material consistency can be achieved by selection and use of one or more of the following: i) the compaction force used to make the preparation; ii) the use of one or more pharmaceutical disintegrants known in the art; iii) use of other pharmaceutical excipients; iv) the particle size and distribution of the preparation (e.g., micronized particles); and v) use of micronizing and other particle formation methods known in the art.

A system 11 for delivery of medication 100 into the wall of the small intestine or other location within the intestinal tract or GI tract, may comprise device 10 which contains one or more medications 100 for the treatment of a selected condition or conditions. In some embodiments, the system may include a hand held device 13, described herein for communicating with device 10 as is shown in the embodiment of FIG. 1b. In many embodiments, system 11 may also be configured as a kit 14 including system 11 and a set of instructions for use 15 which are packaged in packaging 12 as is shown in the embodiment of FIG. 1c. The instructions can indicate to the patient when to take the device 10 relative to one or more events such as the ingestion of a meal or a physiological measurement such as blood glucose, cholesterol, etc. In such embodiments, kit 14 can include multiple devices 10 containing a regimen of medications 100 for a selected period of administration, e.g., a day, week, or multiple weeks depending upon the condition to be treated (e.g., treatment of cancer by a course of interferon treatment, treatment of an autoimmune disease such as psoriasis, multiple sclerosis or arthritis by immune suppression agents).

Capsule 20 is sized to be swallowed and pass through the intestinal tract. The size can also be adjusted depending upon the amount of drug to be delivered as well as the patient's weight and adult vs. pediatric applications. Typically, the capsule will have a tubular shape with curved ends similar to a vitamin. In these and related embodiments, capsule lengths 20L can be in the range of 0.5 to 2 inches and diameters 20D in the range of 0.1 to 0.5 inches with other dimensions contemplated. The capsule 20 includes a capsule wall 21w, having an exterior surface 25 and an interior surface 24 defining an interior space or volume 24v. In some embodiments, the capsule wall 21w can include one or more apertures 26 sized for the outward advancement of tissue penetrating members 40. In addition to the other components of device 10, (e.g., the expandable member etc.) the interior volume can include one or more compartments or reservoirs 27.

The capsule can be fabricated from various biodegradable gelatin materials known in the pharmaceutical arts, but can also include various enteric coatings 20c, configured to protect the cap from degradation in the stomach (due to acids etc.), and then subsequently degrade in the higher pH's found in the small intestine or other area of the intestinal tract.

In various embodiments, the capsule **20** can be formed from multiple portions one or more of which may be biodegradable. In many embodiments, capsule **20** can be formed from two portions **20p** such as a body portion **20p''** (herein body **20p''**) and a cap portion **20p'** (herein cap **20p'**), where the cap fits onto the body, e.g., by sliding over or under the body (with other arrangements also contemplated). One portion such as the cap **20p'** can include a first coating **20c'** configured to degrade above a first pH (e.g., pH 5.5) and the second portion such as the body **20p''** can include a second coating **20c''** configured to degrade above a second higher pH (e.g. 6.5). Both the interior **24** and exterior **25** surfaces of capsule **20** are coated with coatings **20c'** and **20c''** so that either portion of the capsule will be substantially preserved until it contacts fluid having the selected pH. For the case of body **20p''** this allows the structural integrity of the body **20p''** to be maintained so as to keep balloon **72** inside the body portion and not deployed until balloon **30** has expanded. Coatings **20c'** and **20c''** can include various methacrylate and ethyl acrylate based coatings such as those manufactured by Evonik Industries under the trade name EUDRAGIT. These and other dual coating configurations of the capsule **20** allows for mechanisms in one portion of capsule **20** to be actuated before those in the other portion of the capsule. This is due to the fact that intestinal fluids will first enter those portions where the lower pH coating has degraded thus actuating triggers which are responsive to such fluids (e.g., degradable valves). In use, such dual coating embodiments for capsule **20** provide for targeted drug delivery to a particular location in the small intestine (or other location in the GI tract), as well as improved reliability in the delivery process. This is due to the fact that deployment of a particular component, such as aligner **60**, can be configured to begin in the upper area of the small intestine (e.g., the duodenum) allowing the capsule to be aligned within the intestine for optimal delivery of the drug (e.g., into the intestinal wall) as well as providing sufficient time for deployment/actuation of other components to achieve drug delivery into the intestinal wall while the capsule is still in the small intestine or other selected location.

As is discussed above, one or more portions of capsule **20** can be fabricated from various biocompatible polymers known in the art, including various biodegradable polymers which in a preferred embodiment can comprise cellulose, gelatin materials PGLA (polylactic-co-glycolic acid). Other suitable biodegradable materials include various enteric materials described herein as well as lactide, glycolide, lactic acid, glycolic acid, para-dioxanone, caprolactone, trimethylene carbonate, caprolactone, blends and copolymers thereof.

Use of biodegradable materials for capsule **20**, including biodegradable enteric materials allows the capsule to degrade in whole or part to facilitate passage through the GI system before, during or after drug delivery. As is described in further detail herein, in various embodiments, capsule **20** can include seams **22** of bio-degradable material so as to controllably degrade into smaller pieces **23** which are more easily passed through the intestinal tract.

In various embodiments, the wall **20w** of the capsule is degradable by contact with liquids in the GI tract for example liquids in the small intestine. In preferred embodiments, the capsule wall is configured to remain intact during passage through the stomach, but then to be degraded in the small intestine. In one or more embodiments, this can be achieved by the use of an outer coating or layer **20c** on the capsule wall **20w**, which only degrades in the higher pH's found in the small intestine and serves to protect the underlying capsule wall from degradation within the stomach before the capsule reaches the small intestine (at which point the drug delivery

process is initiated by degradation of the coating as is described herein). In use, such coatings allow for the targeted delivery of a therapeutic agent in a selected portion of the intestinal tract such as the small intestine.

In various embodiments, capsule **20** can include various radio-opaque, echogenic or other materials for location of the device using one or more medical imaging modalities such as fluoroscopy, ultrasound, MRI, etc. In specific embodiments, all or a portion of the capsule can include radio-opaque/echogenic markers **20m** as is shown in the embodiment of FIGS. **1a** and **1b**. Suitable materials for radio-opaque markers **20m** include barium sulfate, compounds, titanium dioxide and compounds thereof. In use, such materials allow for the location of device **10** in the GI tract, as well as its state of deployment (e.g., a distinctive marker can be positioned on cap **20p'** and another on body **20p''** allowing for determination if the deployment balloon **30** (discussed below) has inflated but the delivery balloon **72** has not). They can also be used allow for the determination of transit times of the device through the GI tract. Such information can be used to titrate dosages of drug for a particular patient, as well as provide information on when they should take a particular drug after an event such as ingestion of a meal in the case of insulin taken for treatment of diabetes. Markers **20m** can also be positioned on the capsule **20** to allow the physician to determine if the capsule is intact, or has broken up.

As is discussed further herein, in many embodiments, one or more of the deployment member **30**, delivery member **72** or deployable aligner **60**, may correspond to an expandable balloon that is shaped and sized to fit within capsule **20**. Accordingly, for ease of discussion, deployment member **30**, delivery member **72** and deployable aligner **60** will now be referred to as balloon **30**, **60** and **72**; however, it should be appreciated that other devices including various expandable devices are also contemplated for these elements and may include for example, various shape memory devices (e.g., an expandable basket made from shape memory biodegradable polymer spires), expandable piezo electric devices, and/or chemically expandable devices having an expanded shape and size corresponding to the interior volume **24v** of the capsule **20**.

One or more of balloons **30**, **60** and **72** can comprise various polymers known in the medical device arts. In preferred embodiments such polymers can comprise one or more types of polyethylene (PE) which may correspond to low density PE (LDPE), linear low density PE (LLDPE), medium density PE (MDPE) and high density PE (HDPE) and other forms of polyethylene known in the art. In one more embodiments using polyethylene, the material may be cross-linked using polymer irradiation methods known in the art so. In particular embodiments radiation-based cross-linking may be used as to control the inflated diameter and shape of the balloon by decreasing the compliance of the balloon material. The amount or radiation may be selected to achieve a particular amount of cross linking to in turn produce a particular amount of compliance for a given balloon, e.g., increased irradiation can be used to produce stiffer less compliant balloon material. Other suitable polymers can include PET (polyethylene terephthalate), silicone and polyurethane. In various embodiments balloons **30**, **60** and **72** may also include various radio-opaque materials known in the art such as barium sulfate to allow the physician to ascertain the position and physical state of the balloon (e.g., un-inflated, inflated or punctured). Balloons **30**, **60** and **72** can be fabricated using various balloon blowing methods known in the balloon catheters arts (e.g., mold blowing, free blowing, etc) to have a shape and size which corresponds approximately to

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the interior volume **24v** of capsule **20**. In various embodiments one or more of balloons **30**, **60** and **72** and various connecting features (e.g., connecting tubes) can have a unitary construction being formed from a single mold. Embodiments employing such unitary construction provide the benefit of improved manufacturability and reliability since fewer joints must be made between one or more components of device **10**.

Suitable shapes for balloons **30**, **60** and **72** include various cylindrical shapes having tapered or curved end portions (an example of such a shape including a hot dog). In some embodiments, the inflated size (e.g., diameter) of one or more of balloons **30**, **60** and **72**, can be larger than capsule **20** so as to cause the capsule to come apart from the force of inflation, (e.g., due to hoop stress). In other related embodiments, the inflated size of one or more of balloons **30**, **60** and **72** can be such that when inflated, i) the capsule **20** has sufficient contact with the walls of the small intestine so as to elicit a peristaltic contraction causing contraction of the small intestine around the capsule, and/or ii) the folds of the small intestine are effaced to allow. Both of these results allow for improved contact between the capsule/balloon surface and the intestinal wall so as deliver tissue penetrating members **40** over a selected area of the capsule and/or delivery balloon **72**. Desirably, the walls of balloons **30**, **60** and **72** will be thin and can have a wall thickness in the range of 0.005 to 0.0001" more preferably, in the range of 0.005 to 0.0001, with specific embodiments of 0.004, 0.003, 0.002, 0.001, and 0.0005). Additionally in various embodiments, one or more of balloon **30**, **60** or **72** can have a nested balloon configuration having an inflation chamber **60IC** and extended finger **60EF** as is shown in the embodiments of FIG. **3c**. The connecting tubing **63**, connecting the inflation chamber **60IC** can be narrow to only allow the passage of gas **68**, while the connecting tubing **36** coupling the two halves of balloon **30** can be larger to allow the passage of water.

As indicated above, the aligner **60** will typically comprise an expandable balloon and for ease of discussion, will now be referred to as aligner balloon **60** or balloon **60**. Balloon **60** can be fabricated using materials and methods described above. It has an unexpanded and expanded state (also referred to as a deployed state). In its expanded or deployed state, balloon **60** extends the length of capsule **20** such that forces exerted by the peristaltic contractions of the small intestine **SI** on capsule **20** serve to align the longitudinal axis **20LA** of the capsule **20** in a parallel fashion with the longitudinal axis **LAI** of the small intestine **SI**. This in turn serves to align the shafts of tissue penetrating members **40** in a perpendicular fashion with the surface of the intestinal wall **IW** to enhance and optimize the penetration of tissue penetrating members **40** into the intestinal wall **IW**. In addition to serving to align capsule **20** in the small intestine, aligner **60** is also configured to push delivery mechanism **70** out of capsule **20** prior to inflation of delivery balloon **72** (as is shown in Fig) so that the delivery balloon and/or mechanism is not encumbered by the capsule. In use, this push out function of aligner **60** improves the reliability for delivery of the therapeutic agent since it is not necessary to wait for particular portions of the capsule (e.g., those overlying the delivery mechanism) to be degraded before drug delivery can occur.

Balloon **60** may be fluidically coupled to one or more components of device **10** including balloons **30** and **72** by means of polymer tube or other fluidic couplings **62** which may include a tube **63** for coupling balloons **60** and **30** and a tube **64** for coupling balloon **60** and balloon **72**. Tube **63** is configured to allow balloon **60** to be expanded/inflated by pressure from balloon **30** (e.g., pressure generated the mix-

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ture of chemical reactants within balloon **30**) and/or otherwise allow the passage of liquid between balloons **30** and **60** to initiate a gas generating chemical reaction for inflation of one or both of balloons **30** and **60**. Tube **64** connects balloon **60** to **72** so as to allow for the inflation of balloon **72** by balloon **60**. In many embodiments, tube **64** includes or is coupled to a control valve **55** which is configured to open at a selected pressure so as to control the inflation of balloon **72** by balloon **60**. Tube **64** may thus comprise a proximal portion **64p** connecting to the valve and a distal portion **64d** leading from the valve. Typically, proximal and distal portions **64p** and **64d** will be connected to a valve housing **58** as is described below.

Valve **55** may comprise a triangular or other shaped section **56** of a material **57** which is placed within a the chamber **58c** of a valve housing **58** (alternately, it may be placed directly within tubing **64**). Section **57** is configured to mechanically degrade (e.g., tears, shears, delaminates, etc.) at a selected pressure so as to allow the passage of gas through tube **64** and/or valve chamber **58c**. Suitable materials **57** for valve **55** can include bees wax or other form of wax and various adhesives known in the medical arts which have a selectable sealing force/burst pressure. Valve fitting **58** will typically comprise a thin cylindrical compartment (made from biodegradable materials) in which section **56** of material **57** is placed (as is shown in the embodiment of FIG. **3b**) so as to seal the walls of chamber **58c** together or otherwise obstruct passage of fluid through the chamber. The release pressure of valve **55** can be controlled through selection of one or more of the size and shape of section **56** as well as the selection of material **57** (e.g., for properties such as adhesive strength, shear strength etc.). In use, control valve **55** allows for a sequenced inflation of balloon **60** and **72** such that balloon **60** is fully or otherwise substantially inflated before balloon **72** is inflated. This, in turn, allows balloon **60** to push balloon **72** along with the rest of delivery mechanism **70** out of capsule **20** (typically from body portion **20p'**) before balloon **72** inflates so that deployment of tissue penetrating members **40** is not obstructed by capsule **20**. In use, such an approach improves the reliability of the penetration of tissue penetrating members **40** into intestinal wall **IW** both in terms of achieving a desired penetration depth and delivering greater numbers of the penetrating members **40** contained in capsule **20** since the advancement of the members into intestinal wall **IW** is not obstructed by capsule wall **20w**.

As is describe above, the inflated length **601** of the aligner balloon **60** is sufficient to have the capsule **20** become aligned with the lateral axis of the small intestine from peristaltic contractions of the intestine. Suitable inflated lengths **601** for aligner **60** can include a range between about 1/2 to two times the length **201** of the capsule **20** before inflation of aligner **60**. Suitable shapes for aligner balloon **60** can include various elongated shapes such as a hotdog like shape. In specific embodiments, balloon **60** can include a first section **60'** and a second section **60''**, where expansion of first section **60'** is configured to advance delivery mechanism **70** out of capsule **20** (typically out of and second section **60''** is used to inflate delivery balloon **72**. In these and related embodiments, first and second sections **60'** and **60''** can be configured to have a telescope-style inflation where first section **60'** inflates first to push mechanism **70** out of the capsule (typically from body portion **20p'**) and second section **60''** inflates to inflate delivery member **72**. This can be achieve by configuring first section **60'** to have smaller diameter and volume than second section **60''** such that first section **60'** inflates first (because of its smaller volume) and with second section **60''** not inflating until first section **60'** has substantially inflated. In one embodi-

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ment, this can be facilitated by use of a control valve 55 (described above) connecting sections 60' and 60" which does not allow passage of gas into section 60" until a minimum pressure has been reached in section 60'. In some embodiments, the aligner balloon can contain the chemical reactants which react upon mixture with water or other liquid from the deploying balloon.

In many embodiments, the deployment member 30 will comprise an expandable balloon, known as the deployment balloon 30. In various embodiments, deployment balloon 30 is configured to facilitate deployment/expansion of aligner balloon 60 by use of a gas, for example, generation of a gas 69 from a chemical. The gas may be generated by the reaction of solid chemical reactants 65, such as an acid 66 (e.g., citric acid) and a base 66 (e.g., potassium bicarbonate, sodium bicarbonate and the like) which are then mixed with water or other aqueous liquid 68. The amount of reactants be chosen using stoichiometric methods to produce a selected pressure in one or more of balloons 30, 60 and 72. The reactants 65 and liquids can be stored separately in balloon 30 and 60 and then brought together in response to a trigger event, such as the pH conditions in the small intestine. The reactants 65 and liquids 68 can be stored in either balloon, however in preferred embodiments, liquid 68 is stored in balloon 30 and reactants 65 in balloon 60. To allow for passage of the liquid 68 to start the reaction and/or the resulting gas 69, balloon 30 may be coupled to aligner balloon 60 by means of a connector tube 63 which also typically includes a separation means 50 such as a degradable valve 50 described below. For embodiments where balloon 30 contains the liquid, tube 63 has sufficient diameter to allow for the passage of sufficient water from balloon 30 to balloon 60 to produce the desired amount of gas to inflate balloon 60 as well inflate balloon 72. Also when balloon 30 contains the liquid, one or both of balloon 30 and tube 63 are configured to allow for the passage of liquid to balloon 60 by one or more of the following: i) the compressive force applied to balloon 30 by peristaltic contractions of the small intestine on the exposed balloon 30; and ii) wicking of liquid through tube 63 by capillary action.

Tube 63 will typically include a degradable separation valve or other separation means 50 which separates the contents of balloon 30, (e.g., water 58) from those of balloon 60 (e.g., reactants 65) until the valve degrades. Valve 50 can be fabricated from a material such as maltose, which is degradable by liquid water so that the valve opens upon exposure to water along with the various liquids in the digestive tract. It may also be made from materials that are degradable responsive to the higher pH's found in the intestinal fluids such as methacrylate based coatings. The valve is desirably positioned at location on tube 63 which protrudes above balloon 30 and/or is otherwise sufficient exposed such that when cap 20p' degrades the valve 50 is exposed to the intestinal liquids which enter the capsule. In various embodiments, valve 50 can be positioned to lie on the surface of balloon 30 or even protrude above it (as is shown in the embodiments of FIGS. 6a and 6b), so that it has clear exposure to intestinal fluids once cap 20p' degrades. Various embodiments of the invention provide a number of structures for a separation valve 50, for example, a beam like structure (where the valve comprises a beam that presses down on tube 63 and/or connecting section 36), or collar type structure (where the valve comprise a collar lying over tube 63 and/or connecting section 36). Still other valve structures are also contemplated.

Balloon 30 has a deployed and a non-deployed state. In the deployed state, the deployment balloon 30 can have a dome shape 30d which corresponds to the shape of an end of the capsule. Other shapes 30s for the deployed balloon 30 are also

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contemplated, such as spherical, tube-shape, etc. The reactants 65 will typically include at least two reactants 66 and 67, for example, an acid such as citric acid and a base such as sodium bicarbonate, which can have about a 1:2 ratio. Other reactants 65 including other acids, e.g., ascorbic acid and bases, e.g., sodium hydroxide are also contemplated. When the valve or other separation means 50 opens, the reactants mix in the liquid and produce a gas such as carbon dioxide which expands the aligner balloon 60 or other expandable member.

In an alternative embodiment shown in FIG. 3b, the deployment balloon 30 can actually comprise a first and second balloon 30' and 30" connected by a tube 36 or other connection means 36 (e.g., a connecting section). Connecting tube 36 will typically include a separation valve 50 that is degradable by a liquid as described above and/or a liquid having a particular pH such as basic pH found in the small intestine (e.g., 5.5 or 6.5). The two balloons 30' and 30" can each have a half dome shape 30hs allowing them to fit into the end portion of the capsule when in the expanded state. One balloon can contain the chemical reactant(s) 65 (e.g., sodium bicarbonate, citric acid, etc.) the other the liquid water 68, so that when the valve is degraded the two components mix to form a gas which inflates one or both balloons 30' and 30" and in turn, the aligner balloon 60.

In yet another alternative embodiment, balloon 30 can comprise a multi-compartment balloon 30mc, that is formed or other constructed to have multiple compartments 30c. Typically, compartments 30c will include at least a first and a second compartment 34 and 35 which are separated by a separation valve 50 or other separation means 50 as is shown in the embodiment of FIG. 4a. In many embodiments, compartments 34 and 35 will have at least a small connecting section 36 between them which is where separation valve 50 will typically be placed. A liquid 68, typically water, can be disposed within first compartment 34 and one or more reactants 65 disposed in second compartment 35 (which typically are solid though liquid may also be used) as is shown in the embodiment of FIG. 4a. When valve 50 opens (e.g., from degradation caused by fluids within the small intestine) liquid 68 enters compartment 35 (or vice versa or both), the reactant(s) 65 mix with the liquid and produce a gas 69 such as carbon dioxide which expands balloon 30 which in turn can be used to expand one or more of balloons 60 and 72.

Reactants 65 will typically include at least a first and a second reactant, 66 and 67 for example, an acid such as citric acid and a base such as sodium bi-carbonate or potassium bi-carbonate. As discussed herein, in various embodiments they may be placed in one or more of balloon 30 (including compartments 34 and 35 or halves 30' and 30") and balloon 60. Additional reactants, including other combinations of acids and bases which produce an inert gas by product are also contemplated. For embodiments using citric acid and sodium or carbonate, the ratio's between the two reactants (citric acid to potassium bicarbonate) can be in the range of about 1:1 to about 1:4, with a specific ratio of about 1:3. Desirably, solid reactants 65 have little or no absorbed water. Accordingly, one or more of the reactants, such as sodium bicarbonate or potassium bicarbonate can be pre-dried (e.g., by vacuum drying) before being placed within balloon 30. Other reactants 65 including other acids, e.g., ascorbic acid and bases are also contemplated. The amounts of particular reactants 65, including combinations of reactants can be selected to produce particular pressures using known stoichiometric equations for the particular chemical reactions as well as the inflated volume of the balloon and the ideal gas law (e.g.,  $PV=nRT$ ). In particular embodiments, the amounts of reactants can be selected to produce a pressure selected one or

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more of balloons **30**, **60** and **72** to i) achieve a particular penetration depth into the intestinal wall; and produce a particular diameter for one or more of balloons **30**, **60** and **72**; and iii) exert a selected amount of force against intestinal wall IW. In particular embodiments, the amount and ratios of the reactants (e.g., citric acid and potassium bicarbonate) can be selected to achieve pressures in one more of the balloons **30**, **60** and **72** in the range of 10 to 15 psi, with smaller and larger pressures contemplated. Again the amounts and ratio's of the reactants to achieve these pressures can be determined using known stoichiometric equations.

In various embodiments of the invention using chemical reactants **65** to generate gas **69**, the chemical reactants alone or in combination with the deployment balloon **30** can comprise a deployment engine for **80** deploying one or both of the aligner balloon **60** and delivery mechanism **70** including delivery balloon **72**. Deployment engine **80** may also include embodiments using two deployment balloons **30** and **30"** (a dual dome configuration as shown in FIG. **3b**), or a multi compartment balloon **30mc** as shown in FIG. **4a**. Other forms of a deployment engine **80** are also contemplated by various embodiments of the invention such as use of expandable piezo-electric materials (that expand by application of a voltage), springs and other shape memory materials and various thermally expandable materials.

One or more of the expandable balloons **30**, **60** and **72** will also typically include a deflation valve **59** which serves to deflate the balloon after inflation. Deflation valve **59** can comprise biodegradable materials which are configured to degrade upon exposure to the fluids in the small intestine and/or liquid in one of the compartments of the balloon so as to create an opening or channel for escape of gas within a particular balloon. Desirably, deflation valves **59** are configured to degrade at a slower rate than valve **50** to allow sufficient time for inflation of balloons, **30**, **60** and **72** before the deflation valve degrades. In various embodiments, of a compartmentalized balloon **30**, deflation valve **59** can correspond to a degradable section **39** positioned on an end portion **31** of the balloon as is shown in the embodiment of FIG. **4a**. In this and related embodiments, when degradable section **39** degrades from exposure to the liquid, balloon wall **32** tears or otherwise comes apart providing for a high assurance of rapid deflation. Multiple degradable sections **39** can be placed at various locations within balloon wall **32**.

In various embodiments of balloon **72**, deflation valve **59** can correspond to a tube valve **73** attached to the end **72e** of the delivery balloon **72** (opposite to the end which is coupled to the aligner balloon) as is shown in the embodiment of FIG. **3b**. The tube valve **73** comprises a hollow tube **73t** having a lumen that is obstructed at a selected location **73l** with a material **73m** such as maltose that degrades upon exposure to fluid such as the fluid in the small intestine. The location **73l** of the obstructing material **73m** in tube **73t** is selected to provide sufficient time for the delivery balloon **72** to inflate and deliver the tissue penetrating members **40** into the intestinal wall IW before the obstructing material dissolves to open valve **73**. Typically, this will be close to the end **73e** of the tube **73t**, but not quite so as to allow time for liquid to have to wick into the tube lumen before it reaches material **73m**. According to one or more embodiments, once the deflation valve **73** opens, it not only serves to deflate the delivery balloon **72** but also the aligner balloon **60** and deployment balloon **30** since in many embodiments, all three are fluidically connected (aligner balloon being fluidically connected to delivery balloon **72** and the deployment balloon **30** being fluidically connected to aligner balloon **60**). Opening of the deflation valve **73** can be facilitated by placing it on the

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end **72e** of the delivery balloon **72** that is forced out of capsule **20** by inflation of the aligner balloon **60** so that the deflation valve has good exposure to liquids in the small intestine. Similar tube deflation valves **73** can also be positioned on one or both of aligner balloon **62** and the deployment balloon **30**. In these later two cases, the obstructing material in the tube valve can be configured to degrade over a time period to allow sufficient time for inflation of delivery balloon **72** and advancement of tissue penetrating members **40** into the intestinal wall.

Additionally, as further backup for insured deflation, one or more puncture elements **82** (shown in FIG. **2a**) can be attached to the inside surface **24** of the capsule such that when a balloon (e.g., balloon **30**, **60**, **72**) fully inflates it contacts and is punctured by the puncture element **82**. Puncture elements **82** can comprise short protrusions from surface **24** having a pointed tip. In another alternative or additional embodiment of a means for balloon deflation, one or more of the tissue penetrating members **40** can be directly coupled to the wall of **72w** of balloon **72** and configured to tear away from the balloon when they detach, tearing the balloon wall in the process.

A discussion will now be presented of tissue penetrating members **40**. Tissue penetrating member **40** can be fabricated from various drugs and other therapeutic agents **101**, one or more pharmaceutical excipients (e.g., disintegrants, stabilizers, etc.) and one or more biodegradable materials which may be used to form the main structural components of tissue penetrating member **40** including shaft **44** and tip **45** discussed below. The later materials can be chosen to confer desired structural and material properties to the penetrating member (for example, column strength for insertion into the intestinal wall, or porosity and hydrophilicity for control the release of drug. Referring now to FIGS. **8a-8f**; in many embodiments, the penetrating member **40** can be formed to have a shaft **44** and a needle tip **45** or other pointed tip **45** so as to readily penetrate tissue of the intestinal wall as shown in the embodiment of FIG. **8a**. In preferred embodiments, tip **45** has a trocar shape as is shown in the embodiment of FIG. **8c**. Tip **45** may comprise various degradable materials (within the body of the tip or as a coating), such as sucrose, maltose or other sugar which increase the hardness and tissue penetrating properties of the tip. Once placed in the intestinal wall, the penetrating member **40** is degraded by the interstitial fluids within the wall tissue so that the drug or other therapeutic agent **101** dissolves in those fluids and is absorbed into the blood stream. One or more of the size, shape and chemical composition of tissue penetrating member **40** can be selected to allow for dissolution and absorption of drug **101** in a matter of seconds, minutes or even hours. Rates of dissolution can be controlled through the use of various disintegrants known in the pharmaceutical arts. Examples of disintegrants include, but are not limited to various starches such as sodium starch glycolate and various cross linked polymers such as carboxymethyl cellulose. The choice of disintegrants can be specifically adjusted for the environment within the wall of the small intestine e.g., blood flow, average number of peristaltic contractions, etc.

Tissue penetrating member **40** will also typically include one or more tissue retaining features **43** such as a barb or hook to retain the penetrating member within the tissue of the intestinal wall IW after advancement. Retaining features **43** can be arranged in various patterns **43p** to enhance tissue retention such as two or more barbs symmetrically or otherwise distributed around and along member shaft **44** as is shown in the embodiments of FIGS. **8a** and **8b**. Additionally, in many embodiments, penetrating member will also include

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a recess or other mating feature **46** for attachment to a coupling component on delivery mechanism **70**.

Tissue penetrating member **40** is desirably configured to be detachably coupled to platform **75** (or other component of delivery mechanism **70**), so that after advancement of the tissue penetrating member **40** into the intestinal wall, the penetrating member detaches from the balloon. Detachability can be implemented by a variety of means including: i) the snugness or fit between the opening **74** in platform **75** and the member shaft **44**; ii) the configuration and placement of tissue retaining features **43** on penetrating member **40**; and iii) the depth of penetration of shaft **44** into the intestinal wall. Using one or more of these factors, penetrating member **40** be configured to detach as a result of balloon deflation (where the retaining features **43** hold the penetrating member **40** in tissue as the balloon deflates or otherwise pulls back away from the intestinal wall) and/or the forces exerted on capsule **20** by a peristaltic contraction of the small intestine.

In a specific embodiment, the detachability and retention of tissue penetrating member **40** in the intestinal wall IW can be enhanced by configuring the tissue penetrating member shaft **44** to have an inverse taper **44t** as is shown in the embodiment of FIG. **8c**. The taper **44t** on the shaft **44** is configured such that the application of peristaltic contractile forces from the intestinal wall on the shaft result in the shaft being forced inward **9** (e.g., squeezed inward). This is due to the conversion by shaft taper **44t** of the laterally applied peristaltic force PF to an orthogonal force OF acting to force the shaft inward into the intestinal wall. In use, such inverse tapered shaft configurations serve to retain tissue penetrating member **40** within the intestinal wall so as to detach from platform **75** (or other component of delivery mechanism **70**) upon deflation of balloon **72**. Inverse tapers may also be used for embodiments of tissue penetrating member **40** which have any number of tip shapes **45** in addition to a trocar tip. In additional embodiments, tissue penetrating members **40** having an inverse tapered shaft may also include one or more retaining features **43** to further enhance the retention of the tissue penetrating member within intestinal wall IW once inserted.

As described above, in various embodiments, tissue penetrating member **40** can be fabricated from a number of drugs and other therapeutic agents **101**. Also according to one or more embodiments, the tissue penetrating member may be fabricated entirely from drug **101** or may have other constituent components as well, e.g., various pharmaceutical excipients (e.g., binders, preservatives, disintegrants, etc.), polymers conferring desired mechanical properties, etc. Further, in various embodiments one or more tissue penetrating members **40** can carry the same or a different drug **101** (or other therapeutic agent) from other tissue penetrating members. The former configuration allows for the delivery of greater amounts of a particular drug **101**, while the later, allows two or more different drugs to be delivered into the intestinal wall at about the same time to facilitate drug treatment regimens requiring substantial concurrent delivery of multiple drugs. In embodiments of device **10**, have multiple delivery assemblies **78** (e.g., two, one on each face of balloon **72**), a first assembly **78'** can carry tissue penetrating members having a first drug **101** and a second assembly **78''** can carry tissue penetrating members having a second drug **101**.

Typically, the drug or other therapeutic agent **101** carried by the tissue penetrating member **40** will be mixed in with a biodegradable material **105** to form tissue penetrating member **40**. Material **105** may include one or more biodegradable polymers such as PGLA, cellulose, as well as sugars such as maltose or other biodegradable material described herein or known in the art. In such embodiments, the penetrating mem-

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ber **40** may comprise a substantially heterogeneous mixture of drug **101** and biodegradable material **105**. Alternatively, the tissue penetrating member **40** may include a portion **41** formed substantially from biodegradable material **105** and a separate section **42** that is formed from or contains drug **101** as shown in the embodiment of FIG. **8d**. In one or more embodiments, section **42** may correspond to a pellet, slug, cylinder or other shaped section **42s** of drug **101**. Shaped section **42s** may be pre-formed as a separate section which is then inserted into a cavity **42c** in tissue penetrating member **40** as is shown in the embodiments of FIGS. **8e** and **8f**. Alternatively section **42s** may be formed by adding of drug preparation **100** to cavity **42c**. In embodiments, where drug preparation **100** is added to cavity **42c**, preparation may be added in as a powder, liquid, or gel which is poured or injected into cavity **42c**. Shaped section **42s** may be formed of drug **101** by itself or a drug preparation containing drug **101** and one or more binders, preservatives, disintegrates and other excipients. Suitable binders include polyethylene glycol (PEG) and other binders known in the art. In various embodiments, the PEG or other binder may comprise in the range of about 10 to 50% weight percent of the section **42s**, with a preferred embodiment of about 30 weight percent. Other binders may include PLGA, Cyclodextrin, Cellulose, Methyl Cellulose, maltose, Dextrin, Sucrose, PGA.

In various embodiments, the weight of tissue penetrating member **40** can range between about 10 to 15 mg, with larger and smaller weights contemplated. For embodiments of tissue penetrating member **40** fabricated from maltose, the weight can range from about 11 to 14 mg. In various embodiments, depending upon the drug **101** and the desired delivered dose, the weight percent of drug in member **40** can range from about 0.1 to about 15%. The weight percent of drug **101** in member **40** can be adjusted depending upon the desired dose as well as to provide for structural and stoichiometric stability to the drug and also to achieve a desired elution profile of the drug. Table 1 lists the dose and weight percent range for a number of drugs which may be delivered by tissue penetrating member **40**.

TABLE 1

	Dose Via Capsule**	% Weight of Drug in the needle
Drug		
Insulin	5-30 Units	2-15%
Exenatide	10 ug	<1%
Liraglutide	0.6 mg	3-6%
Pramlintide	15-120 ug	0.1-1%
Growth Hormone	0.2-1 mg	2-10%
Somatostatin	50-600 ug	0.3-8%
GnRH and Analogs	0.3-1.5 mg	2-15%
Vasopressin	2-10 units	<1%
PTH/Teriparatide	20 ug	1-2%
Interferons and analogs		
1. For Multiple Sclerosis	0.03-0.25 mg	0.1-3%
2. For Hep B and HepC	6-20 ug	0.05-0.2%
Adalimumab	2-4 mg/day	8-12%
Infliximab	5 mg/day	8-12%
Etanercept	3 mg/day	8-12%
Natalizumab	3 mg/day	8-12%

Tissue penetrating member **40** can be fabricated using one or more polymer and pharmaceutical fabrication techniques known in the art. For example, drug **101** (with or without biodegradable material **105**) can be in solid form and then formed into the shape of the tissue penetrating member **40** using molding, compaction or other like method with one or

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more binding agents added. Alternatively, drug **101** and/or drug preparation **100** may be in solid or liquid form and then added to the biodegradable material **105** in liquid form with the mixture then formed into the penetrating member **40** using molding or other forming method known in the polymer arts.

Desirably, embodiments of the tissue penetrating member **40** comprising a drug or other therapeutic agent **101** and degradable material **105** are formed at temperatures which do not produce any substantial thermal degradation of the drug (or other therapeutic agent) including drugs such as various peptides and proteins. This can be achieved through the use of room-temperature curing polymers and room temperature molding and solvent evaporation techniques known in the art. In particular embodiments, the amount of thermally degraded drug or other therapeutic agent within the tissue penetrating member is desirably less than about 10% by weight and more preferably, less than 5% and still more preferably less than 1%. The thermal degradation temperature(s) for a particular drug are either known or can be determined using methods known in the art and then this temperature can be used to select and adjust the particular polymer processing methods (e.g., molding, curing, solvent evaporation methods etc.) to minimize the temperatures and associated level of drug thermal degradation.

A description will be provided of delivery mechanism **70**. Typically, the mechanism will comprise a delivery assembly **78** (containing tissue penetrating members **40**) that is attached to delivery balloon **72** as is shown in the embodiment of FIGS. **6a** and **6b**. Inflation of the delivery balloon provides a mechanical force for engaging delivery assembly **72** outwards from the capsule and into the intestinal wall IW so as to insert tissue penetrating members **40** into the wall. In various embodiments, the delivery balloon **72** can have an elongated shape with two relatively flat faces **72f** connected by an articulated accordion-like body **72b**. The flat faces **72f** can be configured to press against the intestinal wall (IW) upon expansion of the balloon **72** so as to insert the tissue penetrating members (TPMs) **40** into the intestinal wall. TPMs **40** (either by themselves or as part of a delivery assembly **78** described below) can be positioned on one or both faces **72f** of balloon **70** to allow insertion of drug containing TPMs **40** on opposite sides of the intestinal wall. The faces **72f** of balloon **72** may have sufficient surface area to allow for placement of a number of drug containing TPMs **40** on each face.

Referring now to FIG. **9**, a description will now be provided of assembly of delivery assembly **78**. In a first step **300**, one or more tissue penetrating members **40** can be detachably coupled to a biodegradable advancement structure **75** which may correspond to a support platform **75** (also known as platform **75**). In preferred embodiments, platform **75** includes one or more openings **74** for insertion of members **40** as shown in step **300**. Openings **74** are sized to allow for insertion and retention of members **40** in platform **75** prior to expansion of balloon **72** while allowing for their detachment from the platform upon their penetration into the intestinal wall. Support platform **75** can then be positioned within a carrying structure **76** as shown in step **301**. Carrying structure **76** may correspond to a well structure **76** having side walls **76s** and a bottom wall **76b** which define a cavity or opening **76c**. Platform **75** is desirably attached to inside surface of bottom wall **76b** using adhesive or other joining methods known in the art. Well structure **76** can comprise various polymer materials and may be formed using vacuum forming techniques known in the polymer processing arts. In many embodiments, opening **76c** can be covered with a protective film **77** as shown in step **302**. Protective film **77** has properties

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selected to function as a barrier to protect tissue penetrating members **40** from humidity and oxidation while still allowing tissue penetrating members **40** to penetrate the film as is described below. Film **77** can comprise various water and/or oxygen impermeable polymers which are desirably configured to be biodegradable in the small intestine and/or to pass inertly through the digestive tract. It may also have a multi-ply construction with particular layers selected for impermeability to a given substance, e.g., oxygen, water vapor etc. In use, embodiments employing protective film **77** serve to increase the shelf life of therapeutic agent **101** in tissue penetrating members **40**, and in turn, the shelf life of device **10**. Collectively, support platform **75** attached tissue penetrating members **40**, well structure **76**, and film **77** can comprise a delivery assembly **78**. Delivery assemblies **78** having one or more drugs or therapeutic agents **101** contained within tissue penetrating member **40** or other drug delivery means can be pre-manufactured, stored and subsequently used for the manufacture of device **10** at a later date. The shelf life of assembly **78** can be further enhanced by filling cavity **76c** of the sealed assembly **78** with an inert gas such as nitrogen.

Referring back to FIGS. **6a** and **6b**, assemblies **78** can be positioned on one or both faces **72f** of balloon **72**. In preferred embodiments, assemblies **78** are positioned on both faces **72f** (as shown in FIG. **6a**) so as to provide a substantially equal distribution of force to opposite sides of the intestinal wall IW upon expansion of balloon **72**. The assemblies **78** may be attached to faces **72f** using adhesives or other joining methods known in the polymer arts. Upon expansion of balloon **72**, TPMs **40** penetrate through film **77**, enter the intestinal wall IW and are retained there by retaining elements **43** and/or other retaining features of tissue penetrating (e.g., an inverse tapered shaft **44t**) such that they detach from platform **75** upon deflation of balloon **72**.

In various embodiments, one or more of balloons **30**, **60** and **72** can be packed inside capsule **20** in a folded, furled or other desired configuration to conserve space within the interior volume **24v** of the capsule. Folding can be done using preformed creases or other folding feature or method known in the medical balloon arts. In particular embodiments, balloon **30**, **60** and **72** can be folded in selected orientations to achieve one or more of the following: i) conserve space, ii) produce a desired orientation of a particular inflated balloon; and iii) facilitate a desired sequence of balloon inflations. The embodiments shown in FIGS. **5a-5f** illustrate an embodiment of a method of folding and various folding arrangements. However, it should be appreciated that this folding arrangement and the resulting balloon orientations are exemplary and others may also be used. In this and related embodiments, folding can be done manually, by automated machine or a combination of both. Also in many embodiments, folding can be facilitated by using a single multi balloon assembly **7** (herein assembly **7**) comprising balloons **30**, **60**, **70**; valve chamber **58** and assorted connecting tubings **62** as is shown in the embodiments of FIGS. **3a** and **3b**. FIG. **3a** shows an embodiment of assembly **7** having a single dome construction for balloon **30**, while FIG. **3b** shows the embodiment of assembly **7** having dual balloon/dome configuration for balloon **30**. Assembly **7** can be fabricated using a thin polymer film which is vacuum-formed into the desired shape using various vacuum forming and other related methods known in the polymer processing arts. Suitable polymer films include polyethylene films having a thickness in the range of about 0.003 to about 0.010", with a specific embodiment of 0.005". In preferred embodiments, the assembly is fabricated to have a unitary construction so as to eliminate the need for joining one or more components of the assembly (e.g., balloons **30**,

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60, etc). However, it is also contemplated for assembly 7 to be fabricated from multiple portions (e.g., halves), or components (e.g., balloons) which are then joined using various joining methods known in the polymer/medical device arts.

Referring now to FIGS. 5a-5f, 6a-b and 7a-7b, in a first folding step 210, balloon 60 is folded over onto valve fitting 58 with balloon 72 being flipped over to the opposite side of valve fitting 58 in the process (see FIG. 5a). Then in step 211, balloon 72 is folded at a right angle to the folded combination of balloon 60 and valve 58 (see FIG. 5b). Then, in step 212 for dual dome embodiments of balloon 30, the two halves 30' and 30'' of balloon 30 are folded onto each other, leaving valve 50 exposed (see FIG. 5c, for single dome embodiments of balloon 30, is folded over onto itself see FIG. 5e). A final folding step 213 can be done whereby folded balloon 30 is folded over 180° to the opposite side of valve fitting 58 and balloon 60 to yield a final folded assembly 8 for dual dome configurations shown in the FIG. 5e and a final folded assembly 8' for single dome configurations shown in FIGS. 5e and 5f. One or more delivery assemblies 78 are then be attached to assembly 8 in step 214 (typically two the faces 72f of balloon 72) to yield a final assembly 9 (shown in the embodiments of FIGS. 6a and 6b) which is then inserted into capsule 20. After an insertion step 215, the final assembled version of device 10 with inserted assembly 9 is shown FIGS. 7a and 7b.

Referring now to FIGS. 10a-10i, a description will be provided of a method of using device 10 to deliver medication 101 to a site in the GI tract such as the wall of the small or large intestine. It should be appreciated that the steps and there order is exemplary and other steps and orders also contemplated. After device 10 enters the small intestine SI, the cap coating 20c' is degraded by the basic pH in the upper small intestine causing degradation of cap 20p' as shown in step 400 in FIG. 10b. Valve 50 is then exposed to fluids in the small intestine causing the valve to begin degrade as is shown in step 401 in FIG. 10c. Then, in step 402, balloon 30 expands (due to generation of gas 69) as shown in FIG. 10d. Then, in step 403, section 60' of balloon 60 begins to expand to start to push assembly 78 out of the capsule body as shown in FIG. 10e. Then, in step 404, sections 60' and 60'' of balloon 60 become fully inflated to completely push assembly 78 out of the capsule body extending the capsule length 201 so as to serve to align capsule lateral axis 20AL with the lateral axis of the small intestine LAI as shown in FIG. 10f. During this time, valve 55 is beginning to fail from the increased pressure in balloon 60 (due to the fact that the balloon has fully inflated and there is no other place for gas 69 to go). Then, in step 405, valve 55 has completely opened, inflating balloon 72 which then pushes the now completely exposed assembly 78 (having been pushed completely out of body 20p'') radially outward into the intestinal wall IW as shown in FIG. 10g. Then, in step 406, balloon 72 continues to expand to now advance tissue penetrating members into the intestinal wall IW as shown in FIG. 10h. Then, in step 407, balloon 72, (along with balloons 60 and 30) has deflated pulling back and leaving tissue penetrating members retained in the intestinal wall IW. Also, the body portion 20p'' of the capsule has completely degraded (due to degradation of coating 20c'') along with other biodegradable portions of device 10. Any portion not degraded is carried distally through the small intestine by peristaltic contraction from digestion and is ultimately excreted.

Referring to back FIG. 1b, as an alternative or supplement to the use of pH sensitive degradable coatings and valves for inflation of one or more of balloons 30, 60, and 72 (and deployment of medication 100), in various embodiments the balloons can be expanded responsive to a sensor 97, such as a

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pH sensor 98 or other chemical sensor which detects the presence of the capsule in the small intestine. Sensor 97 can then send a signal to a controllable embodiment of isolation valve 50 or to an electronic controller 29c coupled to a controllable isolation valve 50 to open and thus expand balloon 30 as is described herein. Embodiments of a pH sensor 98 can comprise an electrode-based sensor or it can be a mechanically-based sensor such as a polymer which shrinks or expands upon exposure to a selected pH or other chemical conditions in the small intestine. In related embodiments, an expandable/contractible pH sensor 98 can also comprise the isolation valve 50 itself, by configuring the sensor to expand or contract about connector 63 and/or 36 so as to open a channel between balloons 30 and 60 and/or compartments 34 and 35.

According to another embodiment for detecting when device 10 is in the small intestine (or other location in the GI tract), sensor 97 can comprise pressure/force sensor such as strain gauge for detecting the number of peristaltic contractions that capsule 20 is being subject to within a particular location in the intestinal tract (in such embodiments capsule 20 is desirably sized to be gripped by the small intestine during a peristaltic contraction). Different locations within the GI tract have different number of peristaltic contractions. For example, the small intestine has between 12 to 9 contractions per minute with the frequency decreasing down the length of the intestine. Thus, according to one or more embodiments, detection of the number of peristaltic contractions can be used to not only determine if capsule 20 is in the small intestine, but the relative location within the intestine as well. In use, these and related embodiments allow for release of medication 100 at a particular location in the small intestine.

Still referring to FIG. 1b, as an alternative or supplement to internal activation of drug delivery by device 10 (e.g., using a pH sensitive coatings and/or sensor), in some embodiments, the user may externally send a signal to expand one or more of balloon 30, 60 and 72 to deliver medication 100 to the intestinal wall. The signal may be sent by means of RF, magnetic or other wireless signaling means known in the art. In various embodiments, external activation can be achieved by use of a controllable isolation valve 50 for example, an RF controlled miniature solenoid valve or other electro-mechanical control valve (not shown). In other embodiments, a controllable isolation valve 50 may correspond to a miniature magnetically valve such as a magnetically controlled miniature reed switch (not shown). Such electromechanical or magnetic-based valves can be fabricated using mems and other micro manufacturing methods. In these and related embodiments, the user can use a handheld communication device 13 (e.g., a hand held RF device such as a cell phone) as is shown in the embodiment of FIG. 1b, to send a receive signals 17 from device 10. In such embodiments, swallowable device may include a transmitter 28 such as an RF transceiver chip or other like communication device/circuitry. Handheld device 13 may not only includes signaling means, but also means for informing the user when device 10 is in the small intestine or other location in the GI tract. The later embodiment can be implemented through the use of logic resources 29 (e.g., a processor 29) coupled to transmitter 28 to signal to detect and singe to the user when the device is in the small intestine or other location (e.g., by signaling an input from the sensor). Logic resources 29 may include a controller 29c (either in hardware or software) to control one or more aspects of the process. The same handheld device can also be configured to alert the user when balloon 30 (as well as balloons 52 and 60) has been expanded and the selected medication 100 delivered

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(e.g., using processor 29 and transmitter 28). In this way, the user is provided confirmation that medication 100 has been delivered. This allows the user to take other appropriate drugs/therapeutic agents as well as make other related decisions (e.g., for diabetics to eat a meal or not and what foods should be eaten). The handheld device can also be configured to send a signal to swallowable device 10 to over-ride isolation valve 50 and so prevent, delay or accelerate the delivery of medication 100. In use, such embodiments allow the user to intervene to prevent, delay or accelerate the delivery of medication, based upon other symptoms and/or patient actions (e.g., eating a meal, deciding to go to sleep, exercise etc). The user may also externally expand balloon 30 or expandable member 30 at a selected time period after swallowing the capsule. The time period can be correlated to a typical transit time or range of transit times for food moving through the user's GI tract to a particular location in the tract such as the small intestine.

Referring now to FIGS. 11a-11b and 12, in various embodiments, the capsule 20 can include seams 22 comprising biodegradable material which controllably degrade to produce capsule pieces 23 of a selectable size and shape to facilitate passage through the GI tract as is shown in the embodiment of FIGS. 11a and 11b. Seams 22 can also include pores or other openings 22p for ingress of fluids into the seam to accelerate biodegradation as is shown in the embodiment of FIG. 12. Other means for accelerating biodegradation of seams 22 can include pre-stressing the seam and/or including perforations 22f in the seam as is also shown in the embodiment of FIG. 12.

Referring now to FIGS. 13a-13b and 14, in many embodiments seams 22 can also be configured and arranged so as to allow capsule 20 to be broken into smaller pieces by the inflation of balloon 30 or other expandable member 30. In particular embodiments, seams 22 can be oriented with respect to capsule radial perimeter 21, including having a radial pattern 22rp so as to have the capsule break into halves or other fractional pieces along its perimeter. Seams 22 may also be longitudinally-oriented with respect to capsule lateral access 201a to have the capsule break up into lengthwise pieces.

As alternative or additional approach for breaking up capsule 20 by balloon inflation (or expansion of other expandable member 30), capsule 20 can be fabricated from two or more separate joinable pieces 23j (e.g., radial halves) that are joined at a joint 22j formed by seams 22 (which function as an adhesive joint) as shown in the embodiment of FIG. 22. Alternatively, joinable pieces 23j may be merely joined by a mechanical fit such as a snap or press fit.

Suitable materials for seams 22 can include one or more biodegradable materials described herein such as PGLA, glycolic acid etc. Seams 22 can be attached to capsule 20 using various joining methods known in the polymer arts such as molding, hot melt junctions, etc. Additionally for embodiments of capsule 20 which are also fabricated from biodegradable materials, faster biodegradation of seam 22 can be achieved by one or more of the following: i) fabricating the seam from a faster biodegrading material, ii) pre-stressing the seam, or iii) perforating the seam. The concept of using biodegradable seams 22 to produce controlled degradation of a swallowable device in the GI tract can also be applied to other swallowable devices such as swallowable cameras (or other swallowable imaging device) to facilitate passage through the GI tract and reduce the likelihood of such a device becoming stuck in the GI tract. Accordingly, embodiments of biodegradable seam 22 can be adapted for swallowable imaging and other swallowable devices.

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In still other embodiments, seam 22 can be constructed of materials and/or have a structure which is readily degraded by absorption of ultrasound energy, e.g. high frequency ultrasound (HIFU), allowing the capsule to be degraded into smaller pieces using externally or endoscopically (or other minimally invasive method) administered ultrasound.

Another aspect of the invention provides methods for the delivery of drugs and other therapeutic agents (in the form of medication 100) into the walls of the GI tract using one or more embodiments of swallowable drug delivery device 10. An exemplary embodiment of such a method will now be described. The described embodiment of drug delivery occurs in the small intestine SI. However, it should be appreciated that this is exemplary and that embodiments of the invention can be used for delivering drug in a number of locations in the GI tract including the stomach and the large intestine. For ease of discussion, the swallowable drug delivery device 10 will sometimes be referred to herein as a capsule. As described above, in various embodiments device 10 may be packaged as a kit 14 within sealed packaging 12 that includes device 10 and a set of instructions for use 15. If the patient is using a handheld device 13, the patient may be instructed to enter data into device 13 either manually or via a bar code 18 (or other identifying indicia 18) located on the instructions 15 or packaging 12. If a bar code is used, the patient would scan the bar code using a bar code reader 19 on device 13. After opening packaging 12, reading the instructions 15 and entering any required data, the patient swallows an embodiment of the swallowable drug delivery device 10. Depending upon the drug, the patient may take the device 10 in conjunction with a meal (before, during or after) or a physiological measurement such as a blood glucose measurement. Capsule 20 is sized to pass through the GI tract and travels through the patient's stomach S and into the small intestine SI through peristaltic action as is shown in the embodiment of FIG. 1e. Once the capsule 10 is in the small intestine, coatings 20c' and 20c'' are degraded by the basic pH in the small intestine (or other chemical or physical condition unique to the small intestine) causing expansion of balloon 30, 60 and 72 or deliver medication 100 into the wall of the small intestine SI according to one or more embodiments of the invention.

After medication delivery, device 10 then passes through the intestinal tract including the large intestine LI and is ultimately excreted. For embodiments having a tearable capsule, the capsule may immediately be broken into smaller pieces by inflation of balloon 30. For embodiments of the capsule 20 having biodegradable seams 22 or other biodegradable portions, the capsule is degraded in the intestinal tract into smaller pieces, to facilitate passage through and excretion from the intestinal tract. In particular embodiments having biodegradable tissue penetrating needles/members 40, should the needle get stuck in the intestinal wall, the needle biodegrades releasing the capsule 20 from the wall.

For embodiments of device 10 including a sensor 97, expansion of balloon 30 or other expandable member 30 can be effectuated by the sensor sending a signal to a controllable embodiment of isolation valve 50 and/or a processor 29/controller 29c coupled to the isolation valve 50. For embodiments of device 10 including external actuation capability, the user may externally expand balloon 30 (as well as balloons 52 and 60) at a selected time period after swallowing the capsule. The time period can be correlated to a typical transit time (e.g., 30 minutes) or range of transit times (e.g., 10 minutes to 2 hrs) for food moving through the user's GI tract to a particular location in the tract such as the small intestine.

One or more embodiments of the above methods can be used for the delivery of preparations **100** containing therapeutically effective amounts of a variety of drugs and other therapeutic agents **101** to treat a variety of diseases and conditions. These include a number of large molecule peptides and proteins which would otherwise require injection due to chemical breakdown in the stomach, e.g., growth hormone, parathyroid hormone, insulin, interferons and other like compounds. Suitable drugs and other therapeutic agents which can be delivered by embodiments of the invention include various chemotherapeutic agents (e.g., interferon), antibiotics, antivirals, insulin and related compounds, glucagon like peptides (e.g., GLP-1, exenatide), parathyroid hormones, growth hormones (e.g., IFG and other growth factors), anti-seizure agents (e.g., Furosimide), antimigraine medication (sumatriptan), immune suppression agents (e.g., cyclosporine) and anti-parasitic agents such as various anti-malarial agents. The dosage of the particular drug can be titrated for the patient's weight, age or other parameter. Also the drug **101** to achieve a desired or therapeutic effect (e.g., insulin for blood glucose regulation, Furosimide for anti-seizure) can be less than the amount required should the drug have been delivered by conventional oral delivery (e.g., a swallowable pill that is digested in the stomach and absorbed through the wall of the small intestine). This is due to the fact that there is no degradation of the drug by acid and other digestive fluids in the stomach and the fact that all, as opposed to only a portion of the drug is delivered into the wall of the small intestine (or other lumen in the gastro-intestinal tract, e.g., large intestine, stomach, etc.). Depending upon the drug **101**, the dose **102** delivered in preparation **100** can be in the range from 100 to 5% of a dose delivered by conventional oral delivery means to achieve a desired therapeutic effect (e.g., blood glucose regulation, seizure regulation, etc.) with even lower amounts contemplated. The particular dose reduction can be titrated based upon the particular drug, the condition to be treated, and the patient's weight, age and condition. For some drugs (with known levels of degradation in the intestinal tract) a standard dose reduction can be employed (e.g., 10 to 20%). Larger amounts of dose reduction can be used for drugs which are more prone to degradation and poor absorption. In this way, the potential toxicity and other side effects (e.g., gastric cramping, irritable bowel, hemorrhage, etc.) of a particular drug or drugs delivered by device **10** can be reduced because the ingested dose is lowered. This in turn, improves patient compliance because the patient has reduction both in the severity and incidence of side effects. Additional benefits of embodiments employing dose reduction of drug **101** include a reduced likelihood for the patient to develop a tolerance to the drug (requiring higher doses) and, in the case of antibiotics, for the patient to develop resistant strains of bacteria. Also, other levels of dose reduction can be achieved for patients undergoing gastric bypass operations and other procedures in which sections of the small intestine have been removed or its working (e.g., digestive) length effectively shortened.

In addition to delivery of a single drug, embodiments of swallowable drug delivery device **10** and methods of their use can be used to deliver a plurality of drugs for the treatment of multiple conditions or for the treatment of a particular condition (e.g., protease inhibitors for treatment HIV AIDs). In use, such embodiments allow a patient to forgo the necessity of having to take multiple medications for a particular condition or conditions. Also, they provide a means for facilitating that a regimen of two or more drugs is delivered and absorbed into the small intestine and thus, the blood stream, at about the same time. Due to difference in chemical makeup,

molecular weight, etc., drugs can be absorbed through the intestinal wall at different rates, resulting in different pharmacokinetic distribution curves. Embodiments of the invention address this issue by injecting the desired drug mixtures at substantially the same time. This in turn, improves the pharmacokinetics and thus the efficacy of the selected mixture of drugs. Additionally, eliminating the need to take multiple drugs is particularly beneficial to patients who have one or more long term chronic conditions including those who have impaired cognitive or physical abilities.

In various applications, embodiments of the above methods can be used to deliver preparations **100** including drugs and therapeutic agents **101** to provide treatment for a number of medical conditions and diseases. The medical conditions and diseases which can be treated with embodiments of the invention can include without limitation: cancer, hormonal conditions (e.g., hypo/hyper thyroid, growth hormone conditions), osteoporosis, high blood pressure, elevated cholesterol and triglyceride, diabetes and other glucose regulation disorders, infection (local or septicemia), epilepsy and other seizure disorders, osteoporosis, coronary arrhythmia's (both atrial and ventricular), coronary ischemia anemia or other like condition. Still other conditions and diseases are also contemplated.

In many embodiments, the treatment of the particular disease or condition can be performed without the need for injecting the drug or other therapeutic agent (or other non-oral form of delivery such as suppositories) but instead, relying solely on the therapeutic agent(s) that is delivered into the wall of the small intestine or other portion of the GI tract. For example, diabetes or another glucose regulation disorder can be treated (e.g., by controlling blood glucose levels) solely through the use of insulin that is delivered into the wall of the small intestine without the need for the patient to ever inject insulin. Similarly, the patient need not take conventional oral forms of a drug or other therapeutic agent, but again rely solely on delivery into the wall of the small intestine using embodiments of the swallowable capsule. In other embodiments, the therapeutic agent(s) delivered into the wall of the small intestine can be delivered in conjunction with an injected dose of the agent(s). For example, the patient may take a daily dose of insulin or compound for blood glucose regulation using the embodiments of the swallowable capsule, but only need take an injected dose every several days or when the patient's condition requires it (e.g., hyperglycemia). The same is true for therapeutic agents that are traditionally delivered in oral form (e.g., the patient can take the swallowable capsule and take the conventional oral form of the agent as needed). The dosages delivered in such embodiments (e.g., the swallowed and injected dose) can be titrated as needed (e.g., using standard dose response curve and other pharmacokinetic methods can be used to determine the appropriate dosages). Also, for embodiments using therapeutic agents that can be delivered by conventional oral means, the dose delivered using embodiments of the swallowable capsule can be titrated below the dosage normally given for oral delivery of the agent since there is little or no degradation of the agent within the stomach or other portion of the intestinal tract (herein again standard dose response curve and other pharmacokinetic methods can be applied).

Various groups of embodiments of preparation **100** containing one or more drugs or other therapeutic agents **101** for the treatment of various diseases and conditions will now be described with references to dosages. It should be appreciated that these embodiments, including the particular therapeutic agents and the respective dosages are exemplary and the preparation **100** can comprise a number of other therapeutic

agents described herein (as well as those known in the art) that are configured for delivery into a luminal wall in the intestinal tract (e.g., the small intestinal wall) using various embodiments of device 10. The dosages can be larger or smaller than those described and can be adjusted using one or more methods described herein or known in the art. In one group of embodiments, therapeutic agent preparation 100 can comprise a therapeutically effective dose of insulin for the treatment of diabetes and other glucose regulation disorders. The insulin can be human or synthetically derived as is known in the art. In one embodiment, preparation 100 can contain a therapeutically effective amount of insulin in the range of about 1-10 units (one unit being the biological equivalent of about 45.5 µg of pure crystalline insulin), with particular ranges of 2-4, 3-9, 4-9, 5-8 or 6-7. The amount of insulin in the preparation can be titrated based upon one or more of the following factors (herein, then “glucose control titration factors”): i) the patient’s condition (e.g., type 1 vs. type II diabetes; ii) the patient’s previous overall level of glycemic control; iii) the patient’s weight; iv) the patient’s age; v) the frequency of dosage (e.g., once vs. multiple times a day); vi) time of day (e.g., morning vs. evening); vii) particular meal (breakfast vs. dinner); viii) content/glycemic index of a particular meal (e.g., meals having a high fat/lipid and sugar content (which tend to cause a rapid rise in blood sugar and thus have a higher glycemic index) vs. low fat and sugar content that do not (and thus have a lower glycemic index)); and ix) content of the patient’s overall diet (e.g., amount of sugars and other carbohydrates, lipids and protein consumed daily).

In another group of embodiments, therapeutic agent preparation 100 can comprise a therapeutically effective dose of one or more incretins for the treatment of diabetes and other glucose regulation disorders. Such incretins can include Glucagon like peptide 1 (GLP-1) and their analogues, and Gastric inhibitory peptide (GIP). Suitable GLP-1 analogues include exenatide, liraglutide, albiglutide and taspoglutide as well as their analogues, derivatives and other functional equivalents. In one embodiment preparation 100 can contain a therapeutically effective amount of exenatide in the range of about 1-10 µg, with particular ranges of 2-4, 4-6, 4-8 and 8-10 µg respectively. In another embodiment, preparation 100 can contain a therapeutically effective amount of liraglutide in the range of about 1-2 mg (milligrams), with particular ranges of 1.0 to 1.4, 1.2 to 1.6 and 1.2 to 1.8 mg respectively. One or more of the glucose control titration factors can be applied to titrate the dose ranges for exenatide, liraglutide or other GLP-1 analogue or incretin.

In yet another group of embodiments, therapeutic agent preparation 100 can comprise a combination of therapeutic agents for the treatment of diabetes and other glucose regulation disorders. Embodiments of such a combination can include therapeutically effective doses of incretin and biguanide compounds. The incretin can comprise one or more GLP-1 analogues described herein, such as exenatide and the biguanide can comprise metformin (e.g., that available under the Trademark of GLUCOPHAGE manufactured by Merck Santé S.A.S.) and its analogues, derivatives and other functional equivalents. In one embodiment, preparation 100 can comprise a combination of a therapeutically effective amount of exenatide in the range of about 1-10 µg and a therapeutically effective amount of metformin in a range of about 1 to 3 grams. Smaller and larger ranges are also contemplated with one or more of the glucose control titration factors used to titrate the respective dose of exenatide (or other incretin) and metformin or other biguanide. Additionally, the dosages of the exenatide or other incretin and metformin or other bigu-

anide can be matched to improve the level of glucose control for the patient (e.g., maintenance of blood glucose within normal physiological levels and/or a reduction in the incidence and severity of instances of hyperglycemia and/or hypoglycemia) for extended periods of time ranging from hours (e.g., 12) to a day to multiple days, with still longer periods contemplated. Matching of dosages can also be achieved by use of the glucose control regulation factors as well as monitoring of the patient’s blood glucose levels for extended periods using glycosylated hemoglobin (known as hemoglobin A1c, HbA1c, A1C, or Hb1c) and other analytes and measurements correlative to long term average blood glucose levels.

In still yet another group of embodiments, therapeutic agent preparation 100 can comprise a therapeutically effective dose of growth hormone for the treatment of one or more growth disorders, as well as wound healing. In one embodiment, preparation 100 can contain a therapeutically effective amount of growth hormone in the range of about 0.1-4 mg, with particular ranges of 0.1-1, 1-4, 1-2 and 2-4, with still larger ranges contemplated. The particular dose can be titrated based on one or more of the following: i) the particular condition to be treated and its severity (e.g., stunted growth, vs. wound healing); ii) the patient’s weight; iii) the patient’s age; and iv) the frequency of dosage (e.g., daily vs. twice daily).

In still yet another group of embodiments, therapeutic agent preparation 100 can comprise a therapeutically effective dose of parathyroid hormone for the treatment osteoporosis or a thyroid disorder. In one embodiment, preparation 100 can contain a therapeutically effective amount of parathyroid hormone in the range of about 1-40 µg, with particular ranges of 10-20, 20-30, 30-40 and 10-40 µg, with still larger ranges contemplated. The particular dose can be titrated based on one or more of the following: i) the particular condition to be treated and its severity (e.g., the degree of osteoporosis as determined by bone density measurements); ii) the patient’s weight; iii) the patient’s age; and iv) the frequency of dosage (e.g., daily vs. twice daily).

The foregoing description of various embodiments of the invention has been presented for purposes of illustration and description. It is not intended to limit the invention to the precise forms disclosed. Many modifications, variations and refinements will be apparent to practitioners skilled in the art. For example, embodiments of the device can be sized and otherwise adapted for various pediatric and neonatal applications as well as various veterinary applications. Also those skilled in the art will recognize, or be able to ascertain using no more than routine experimentation, numerous equivalents to the specific devices and methods described herein. Such equivalents are considered to be within the scope of the present invention and are covered by the appended claims below.

Elements, characteristics, or acts from one embodiment can be readily recombined or substituted with one or more elements, characteristics or acts from other embodiments to form numerous additional embodiments within the scope of the invention. Moreover, elements that are shown or described as being combined with other elements, can, in various embodiments, exist as standalone elements. Hence, the scope of the present invention is not limited to the specifics of the described embodiments, but is instead limited solely by the appended claims.

What is claimed is:

1. A swallowable device for oral delivery of a therapeutic agent into an intestinal wall of a patient’s intestinal tract, the device comprising:

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a swallowable capsule sized to pass through the intestinal tract, the capsule having a degradable capsule wall, a portion of which degrades upon exposure to a selected pH in the intestine while protecting the capsule wall from degradation in the stomach;

a deployable aligner disposed and deployable from within the capsule to extend a length of the capsule, in its deployed state, the aligner having an elongated shape and a length with respect to a longitudinal axis of the capsule that are configured to extend the length of the capsule so as to align the longitudinal axis of the capsule with a longitudinal axis of the intestine, by application of peristaltic force on the length of the aligner, for the delivery of the therapeutic agent into the intestinal wall;

a delivery mechanism for delivering the therapeutic agent into the intestinal wall; and;

a deployment engine for deploying the delivery mechanism and the deployable aligner.

2. The device of claim 1, wherein the aligner comprises an expandable balloon.

3. The device of claim 1, wherein the aligner has a hot-dog like shape.

4. The device of claim 1, wherein the aligner has a length in a range from about one half to about two times the length of the swallowable capsule.

5. The device of claim 1, wherein the delivery mechanism comprises an expandable balloon.

6. The device of claim 1, further comprising at least one tissue penetrating member including a proximal portion detachably coupled to the delivery mechanism, a tissue pen-

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etrating distal portion and a therapeutic agent preparation for delivery into the intestinal wall.

7. The device of claim 6, wherein the therapeutic agent preparation comprises a shaped section disposed within the at least one tissue penetrating member.

8. The device of claim 6, wherein the at least one tissue penetrating member is formed at least in part from the therapeutic agent preparation.

9. The device of claim 6, wherein the at least one tissue penetrating member includes a retaining feature for retaining the tissue penetrating member within the intestinal wall.

10. The device of claim 9, wherein the retaining feature comprises a barb or a hook.

11. The device of claim 9, wherein the at least one tissue penetrating member comprises a plurality of tissue penetrating members.

12. The device of claim 1, wherein the deployment engine comprises an expandable member.

13. The device of claim 12, wherein the deployment engine further comprises at least one chemical reactant disposed in or fluidically coupled to the expandable member.

14. The device of claim 12, wherein the expandable member comprises an expandable balloon.

15. The device of claim 1, wherein the intestine is the small intestine and the capsule wall is configured to degrade in response to a selected pH in the small intestine.

16. The device of claim 15, wherein the pH is equal to or greater than about 6.5.

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